



US009398936B2

(12) **United States Patent**
Razzaque et al.

(10) **Patent No.:** **US 9,398,936 B2**
(45) **Date of Patent:** ***Jul. 26, 2016**

(54) **SYSTEMS, METHODS, APPARATUSES, AND
COMPUTER-READABLE MEDIA FOR
IMAGE GUIDED SURGERY**

(71) Applicant: **InnerOptic Technology, Inc.,**
Hillsborough, NC (US)

(72) Inventors: **Sharif Razzaque**, Chapel Hill, NC (US);
John Martinie, Charlotte, NC (US);
David Iannitti, Charlotte, NC (US);
Andrei State, Chapel Hill, NC (US);
Brian Heaney, Durham, NC (US)

(73) Assignee: **INNEROPTIC TECHNOLOGY, INC.,**
Hillsborough, NC (US)

(*) Notice: Subject to any disclaimer, the term of this
patent is extended or adjusted under 35
U.S.C. 154(b) by 66 days.

This patent is subject to a terminal dis-
claimer.

(21) Appl. No.: **14/166,173**

(22) Filed: **Jan. 28, 2014**

(65) **Prior Publication Data**

US 2014/0142425 A1 May 22, 2014

Related U.S. Application Data

(63) Continuation of application No. 12/703,118, filed on
Feb. 9, 2010, now Pat. No. 8,690,776.

(60) Provisional application No. 61/207,593, filed on Feb.
17, 2009, provisional application No. 61/207,589,
filed on Feb. 17, 2009, provisional application No.
61/207,592, filed on Feb. 17, 2009.

(51) **Int. Cl.**

A61B 19/00 (2006.01)

A61B 8/00 (2006.01)

(Continued)

(52) **U.S. Cl.**

CPC **A61B 19/5244** (2013.01); **A61B 8/4245**
(2013.01); **A61B 18/02** (2013.01);

(Continued)

(58) **Field of Classification Search**

CPC A61B 5/05; A61B 8/4245
See application file for complete search history.

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Primary Examiner — Peter Luong

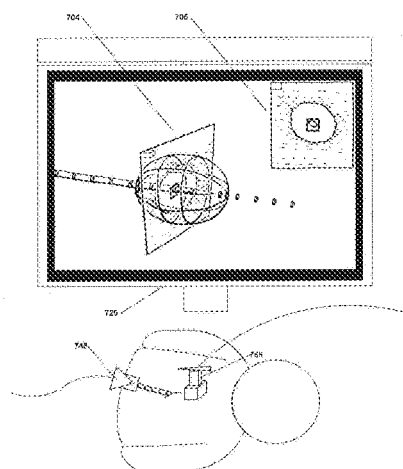
(74) *Attorney, Agent, or Firm* — Knobbe, Martens, Olson &
Bear, LLP

(57)

ABSTRACT

Presented herein are methods, systems, devices, and com-
puter-readable media for image guided surgery. The systems
herein allow a physician to use multiple instruments for a
surgery and simultaneously provide image-guidance data for
those instruments. Various embodiments disclosed herein
provide information to physicians about procedures they are
performing, the devices (such as ablation needles, ultrasound
wands or probes, scalpels, cauterizers, etc.) they are using
during the procedure, the relative emplacements or poses of
these devices, prediction information for those devices, and
other information. Some embodiments provide useful infor-
mation about 3D data sets. Additionally, some embodiments
provide for quickly calibratable surgical instruments or
attachments for surgical instruments.

20 Claims, 23 Drawing Sheets



- (51) **Int. Cl.**
- A61B 18/02* (2006.01)
- A61B 18/08* (2006.01)
- A61B 18/14* (2006.01)
- A61B 18/18* (2006.01)
- A61B 18/20* (2006.01)
- (52) **U.S. Cl.**
- CPC *A61B 18/082* (2013.01); *A61B 18/1442* (2013.01); *A61B 18/1477* (2013.01); *A61B 18/18* (2013.01); *A61B 18/20* (2013.01); *A61B 2018/1425* (2013.01); *A61B 2034/102* (2016.02); *A61B 2034/104* (2016.02); *A61B 2034/207* (2016.02); *A61B 2090/368* (2016.02); *A61B 2090/3983* (2016.02); *A61B 2090/502* (2016.02)
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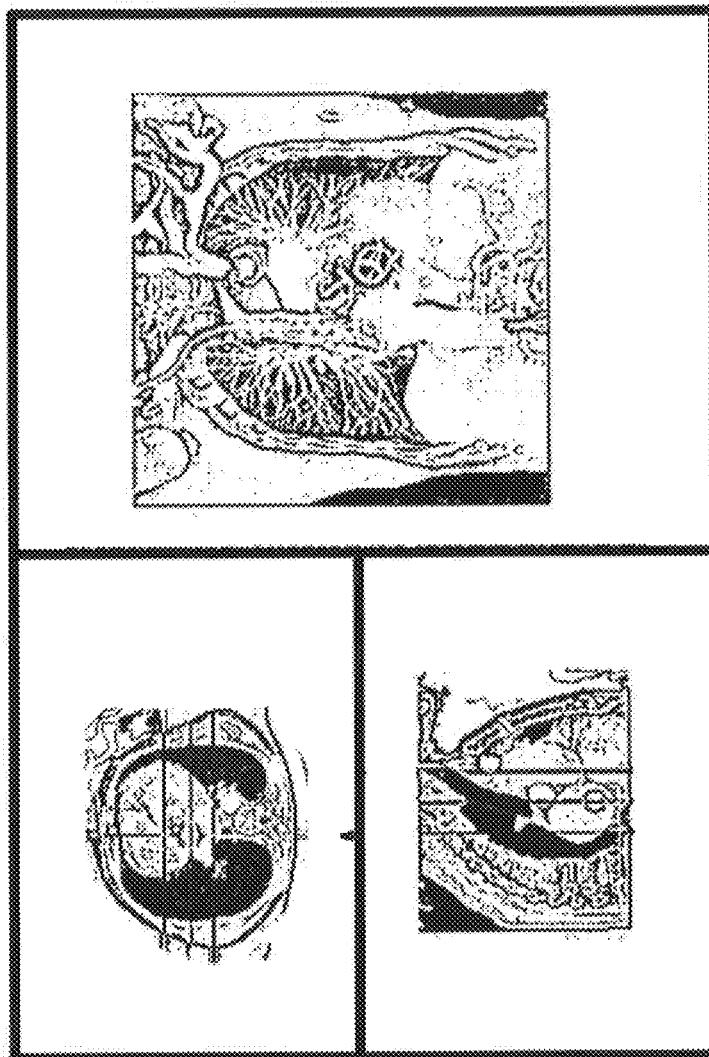


FIGURE 1

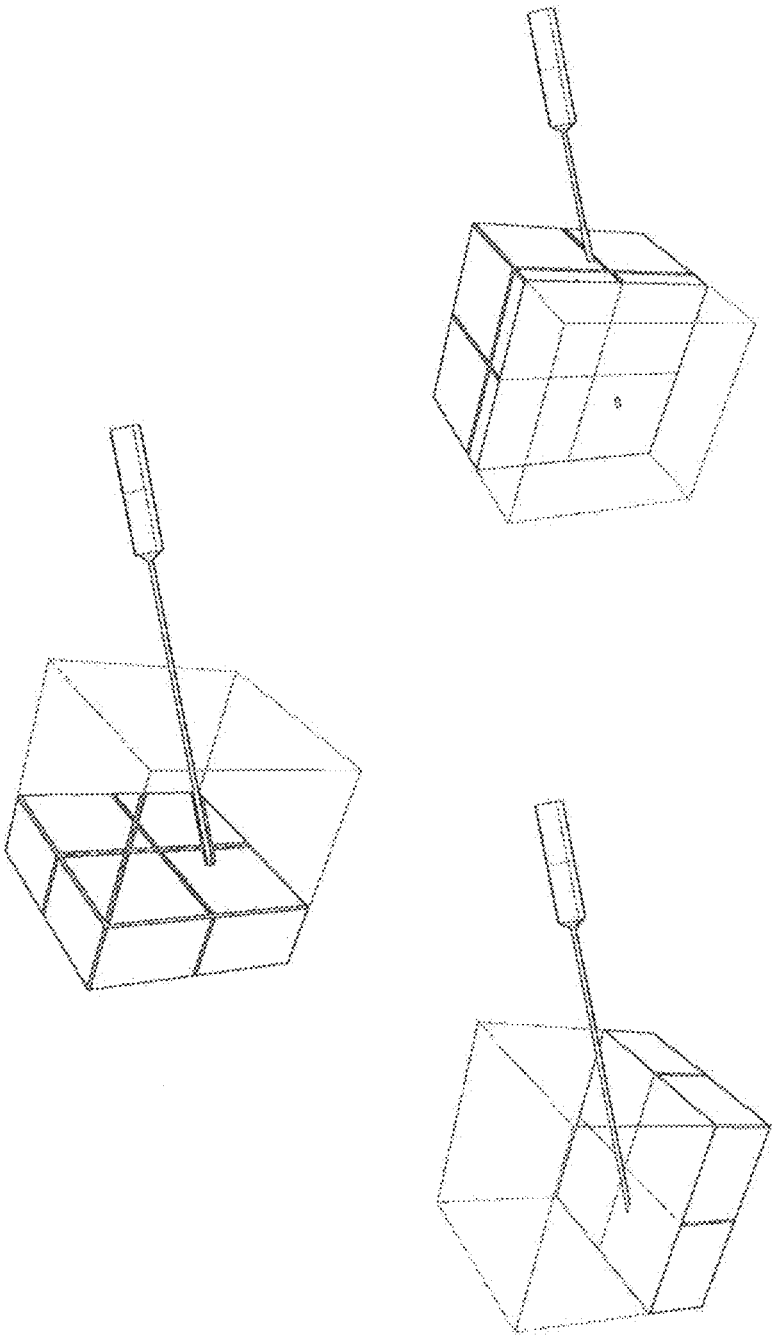


FIGURE 2

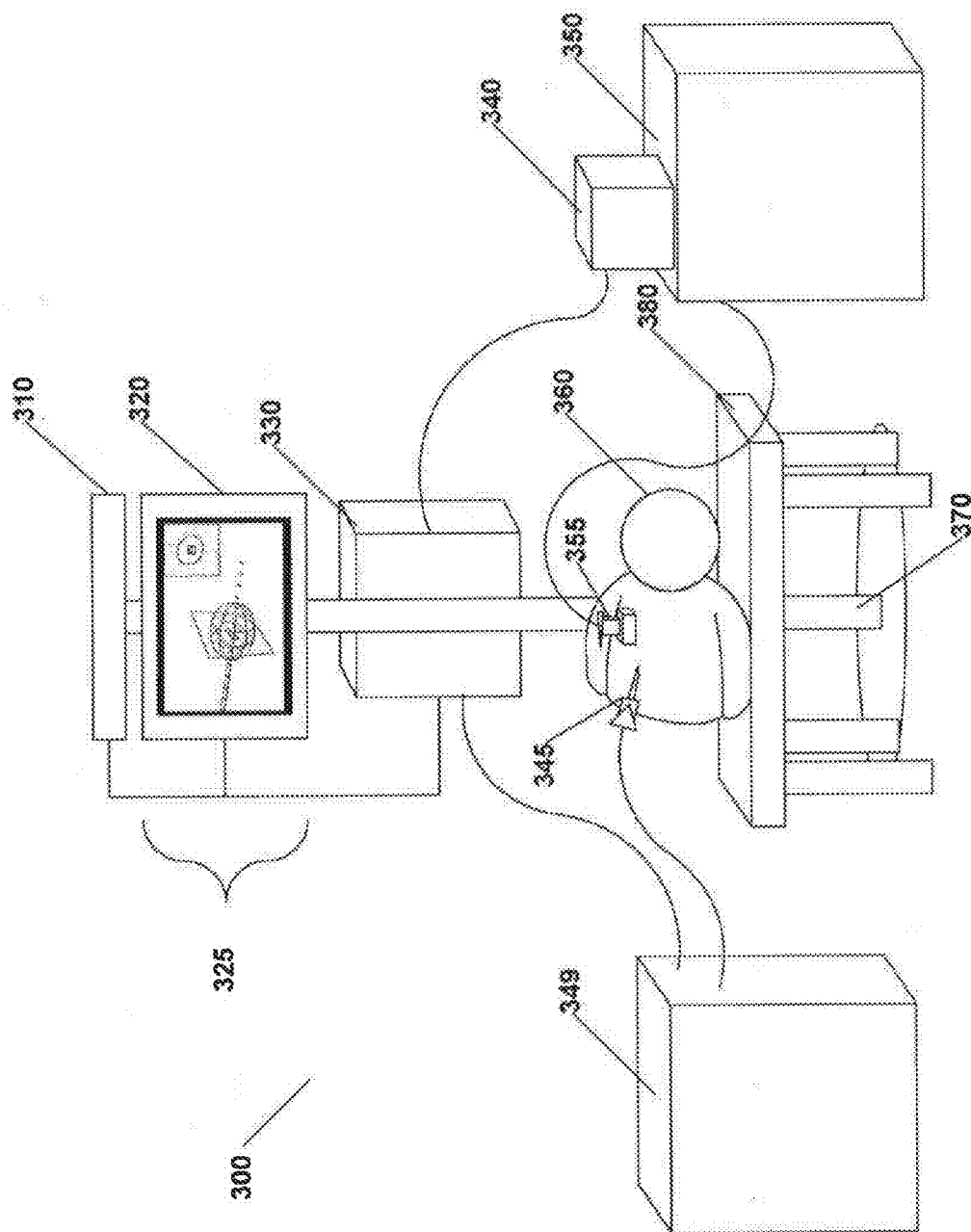


FIGURE 3A

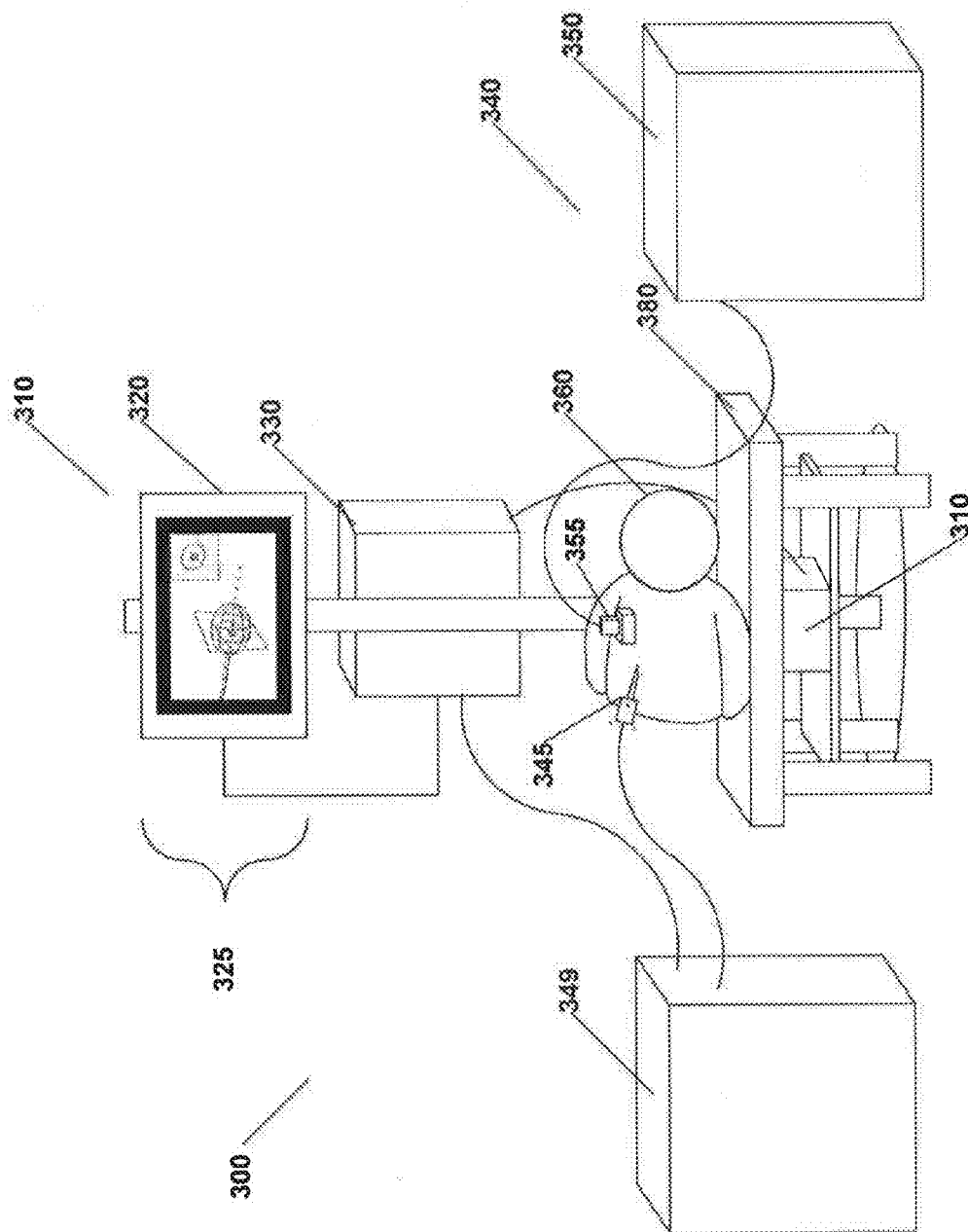
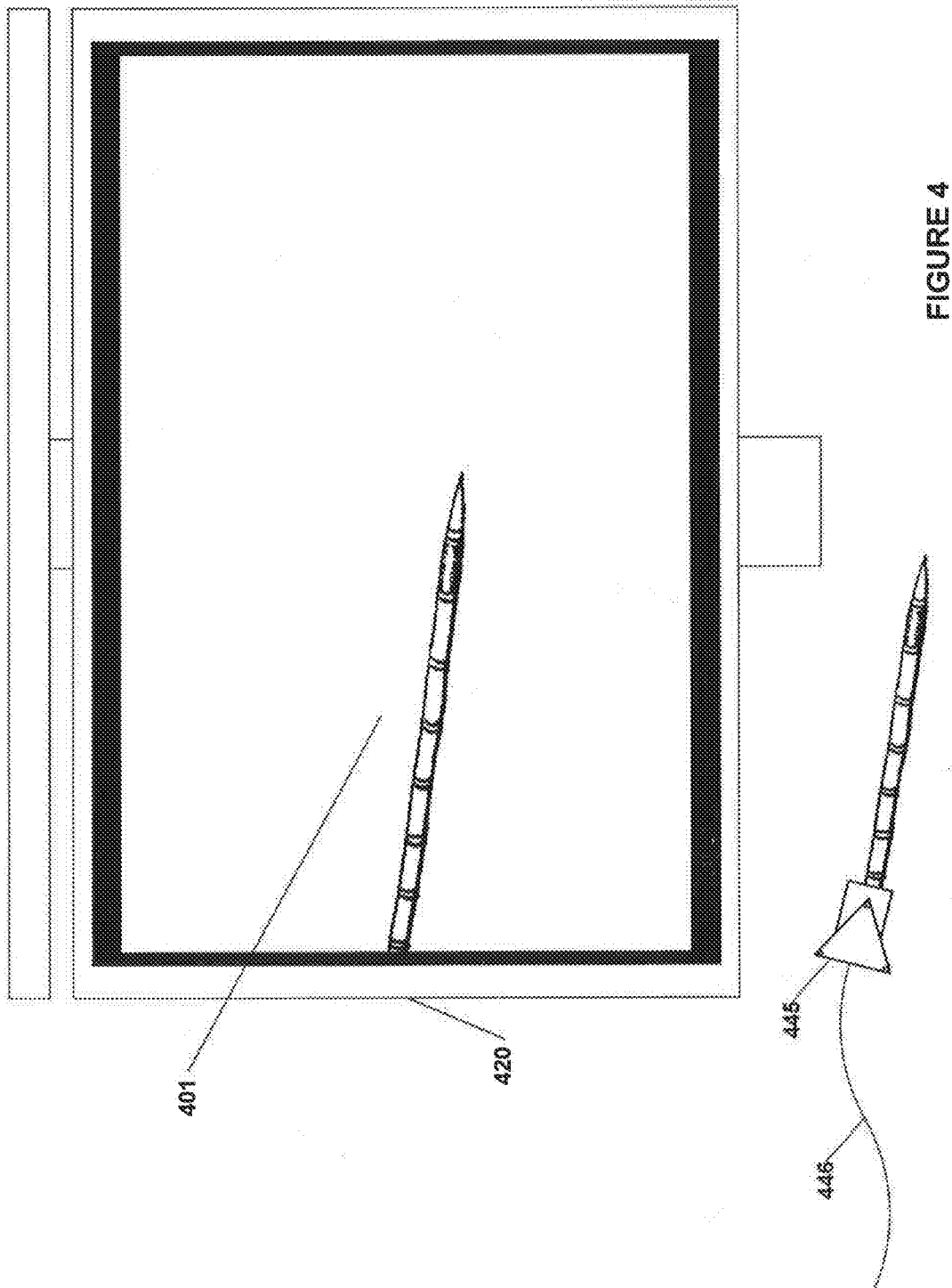


FIGURE 3B



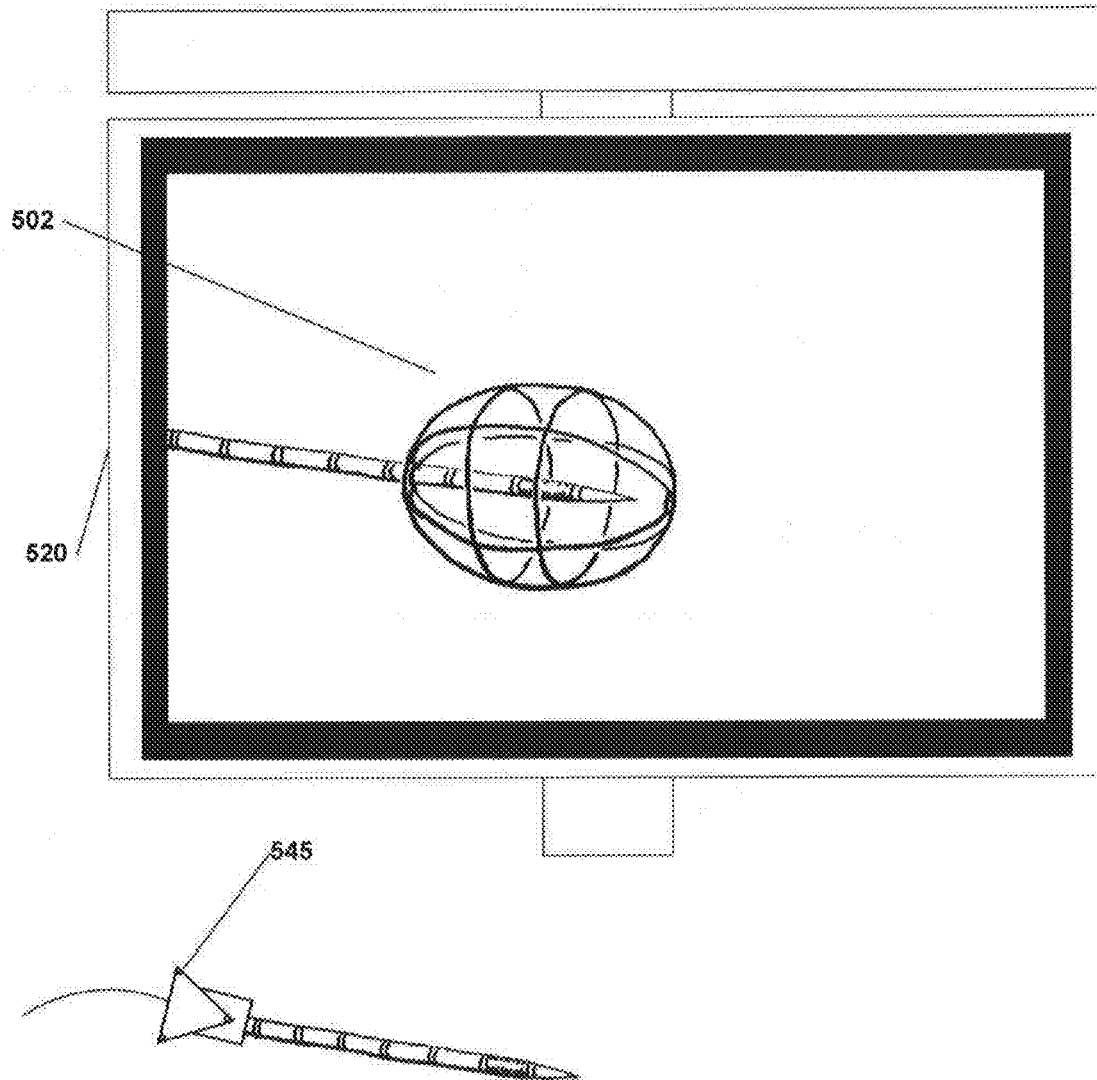


FIGURE 5

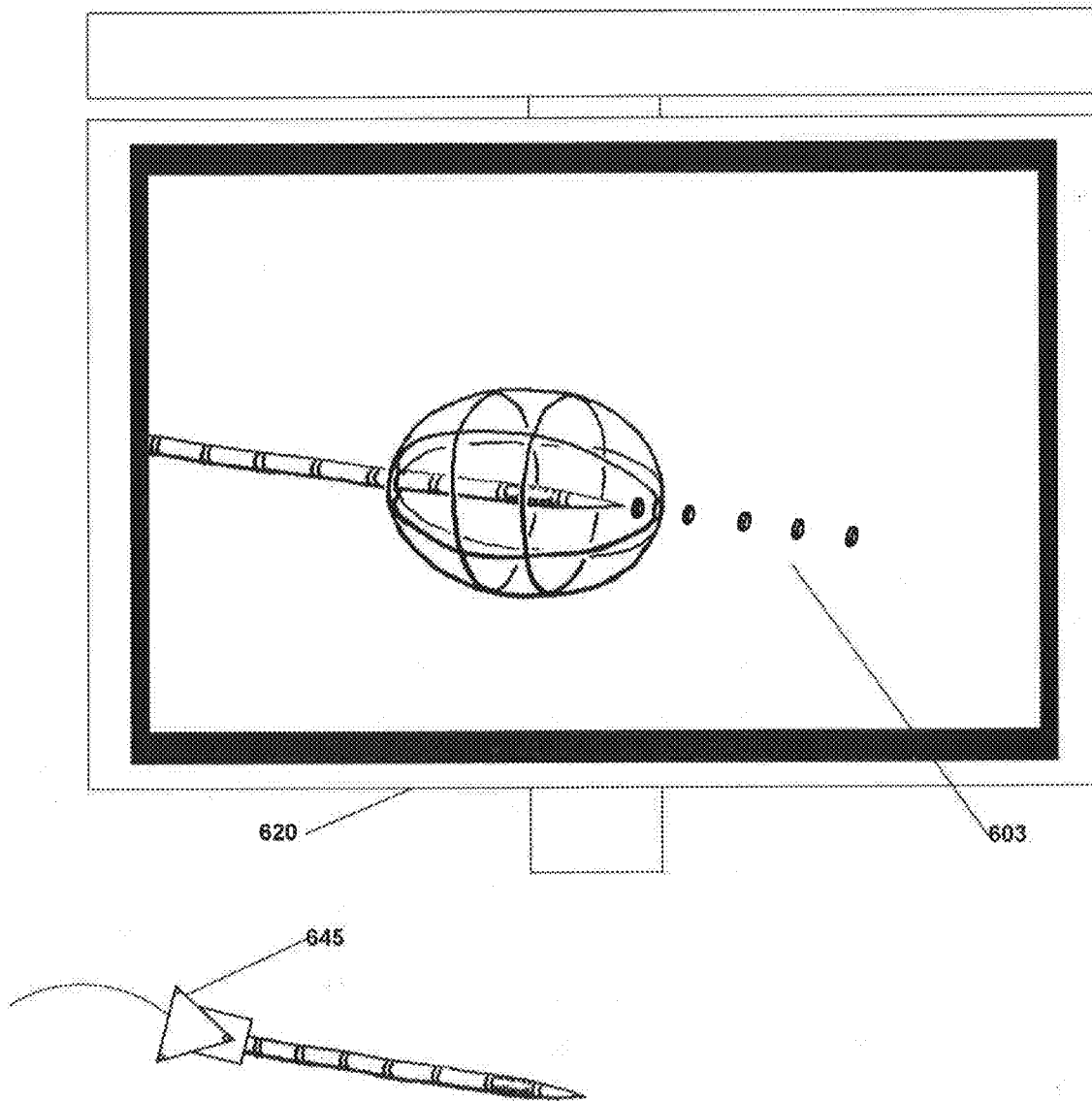


FIGURE 6

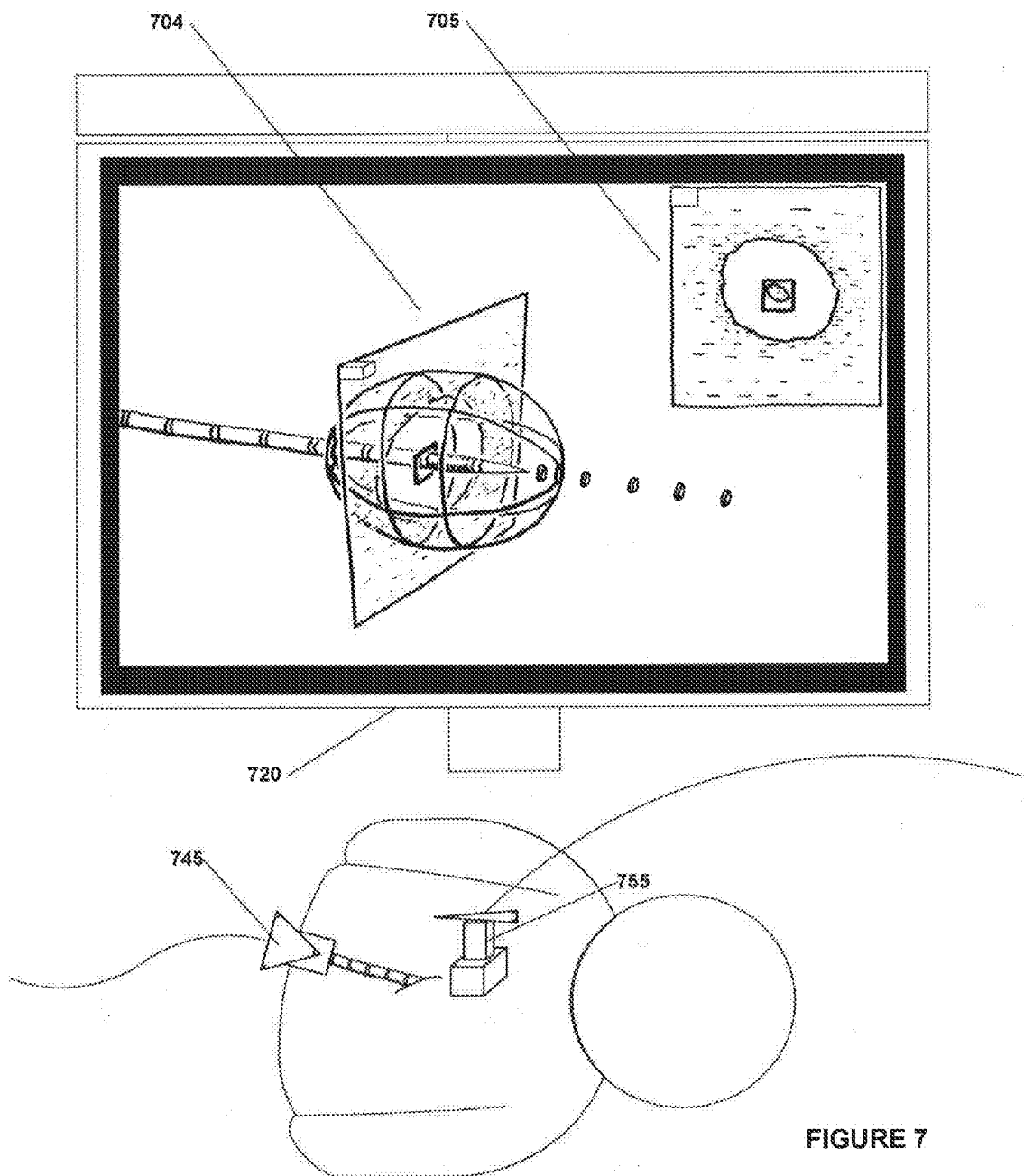


FIGURE 7

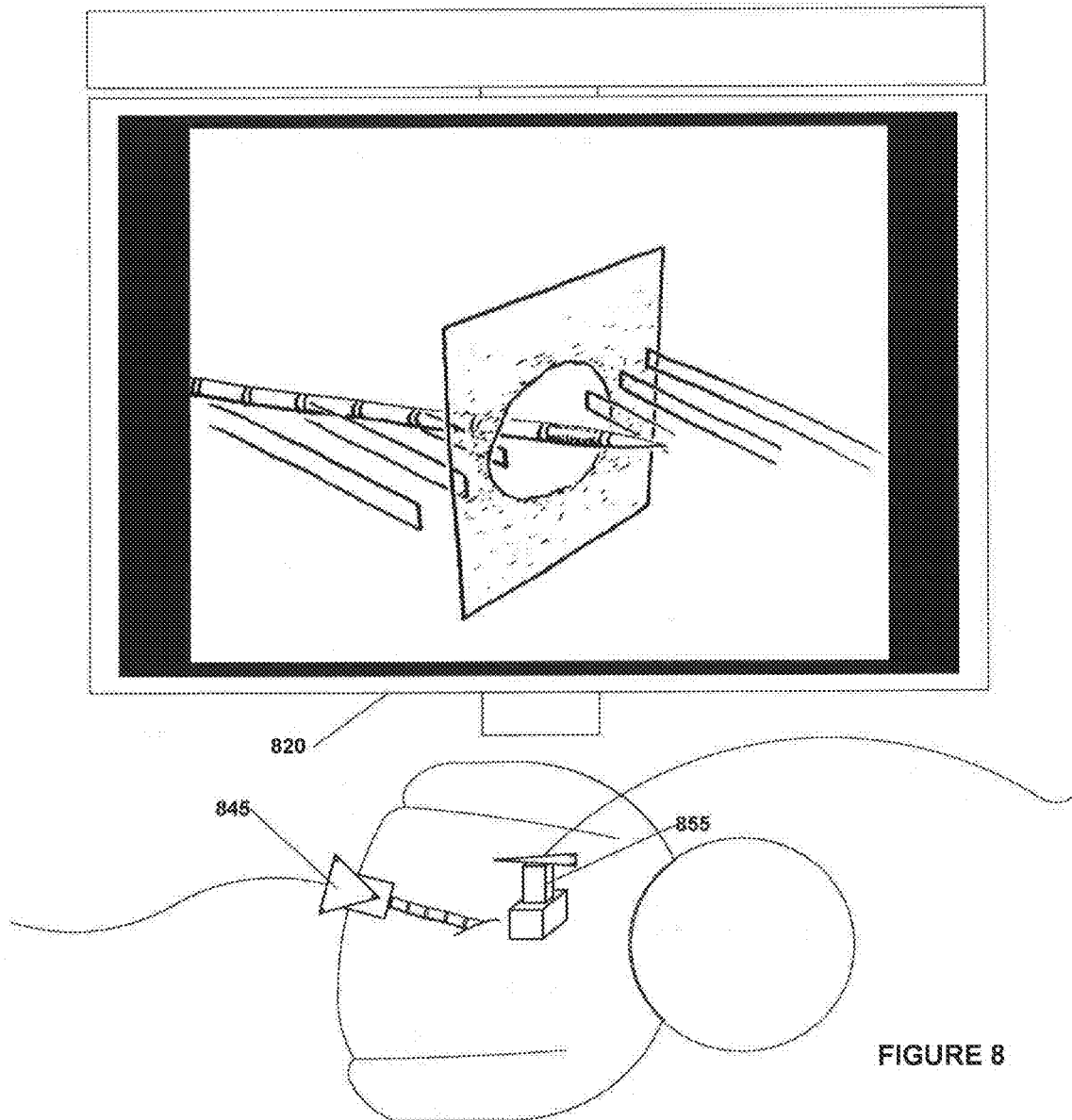
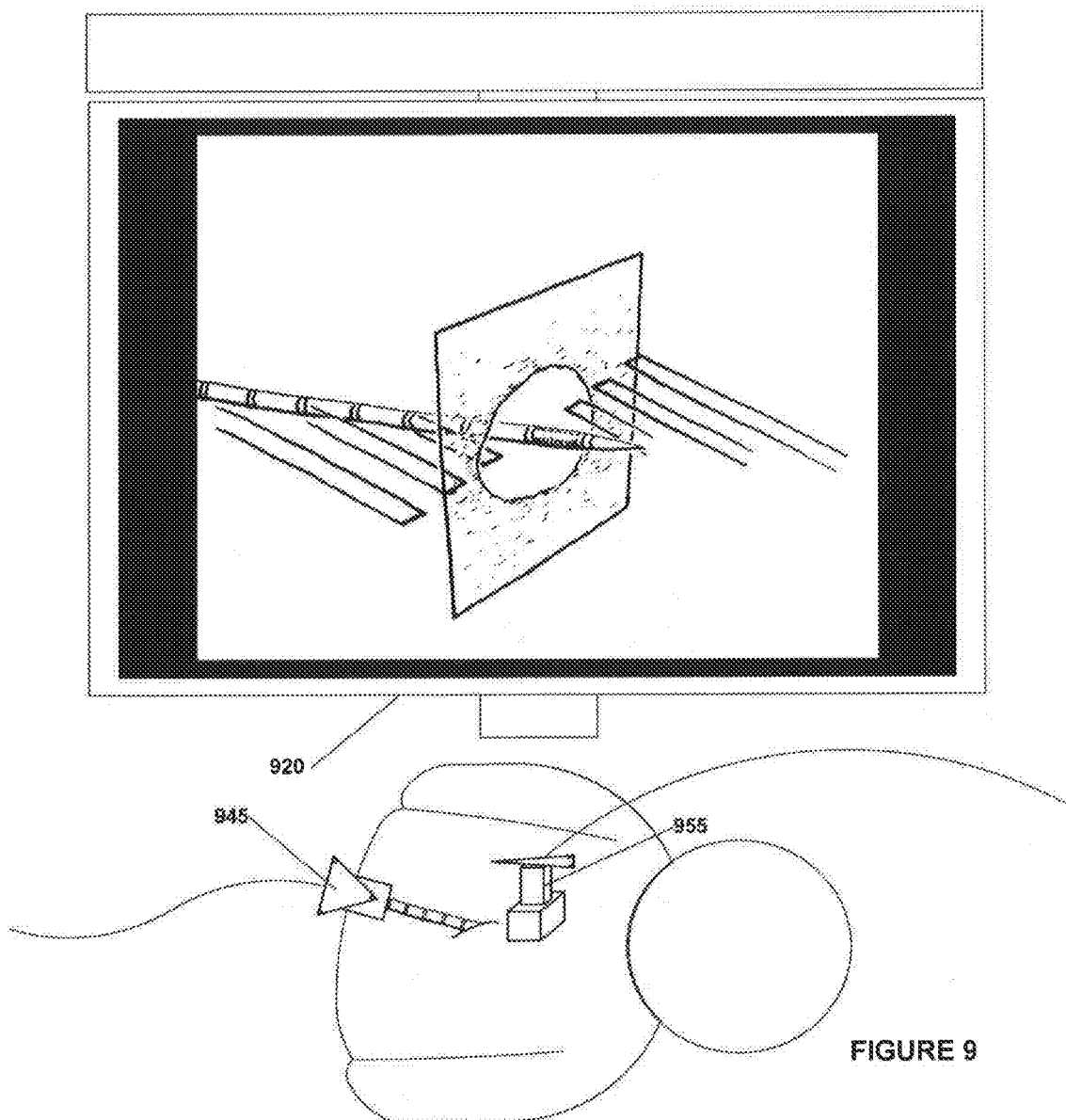


FIGURE 8



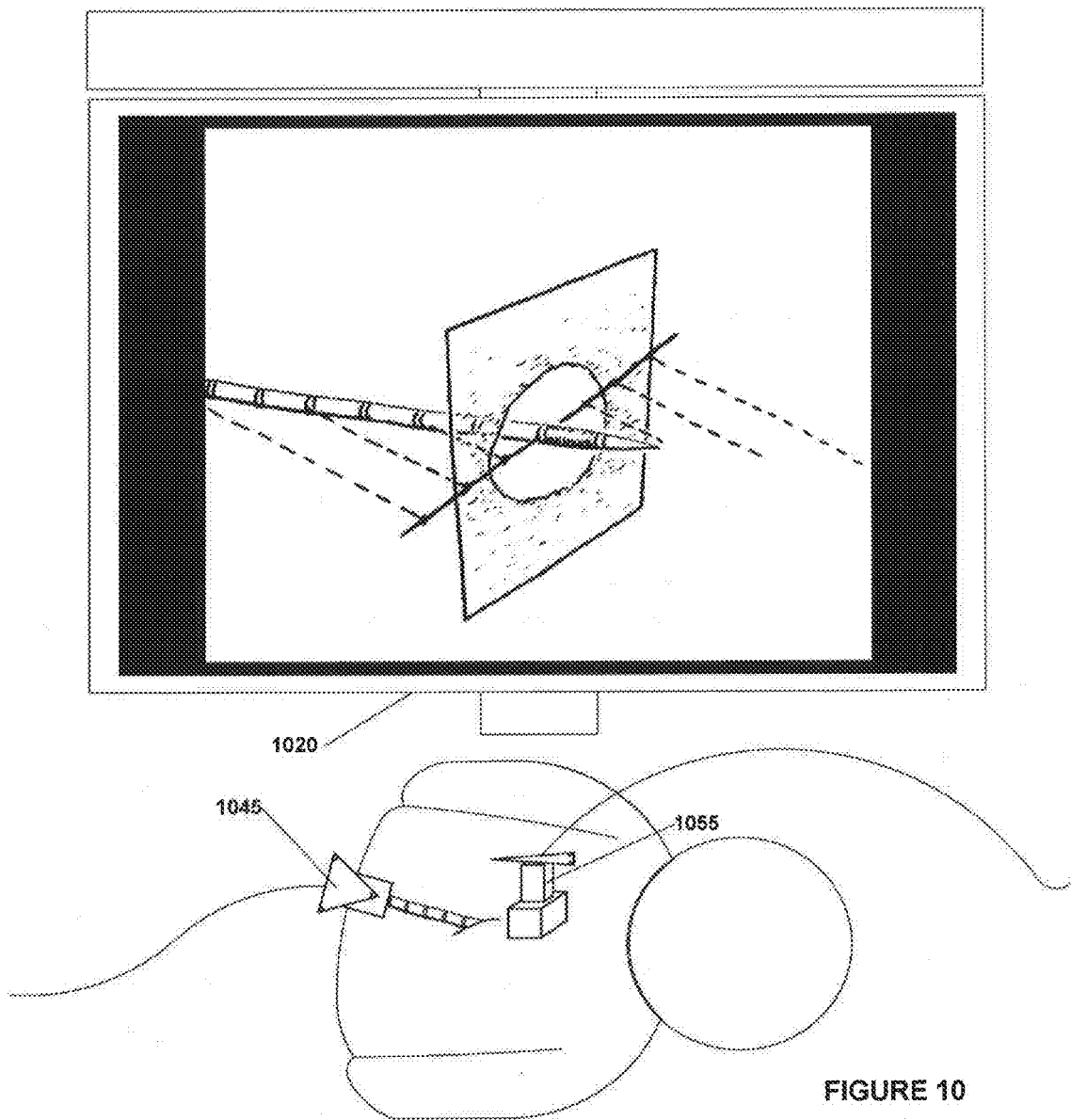


FIGURE 10

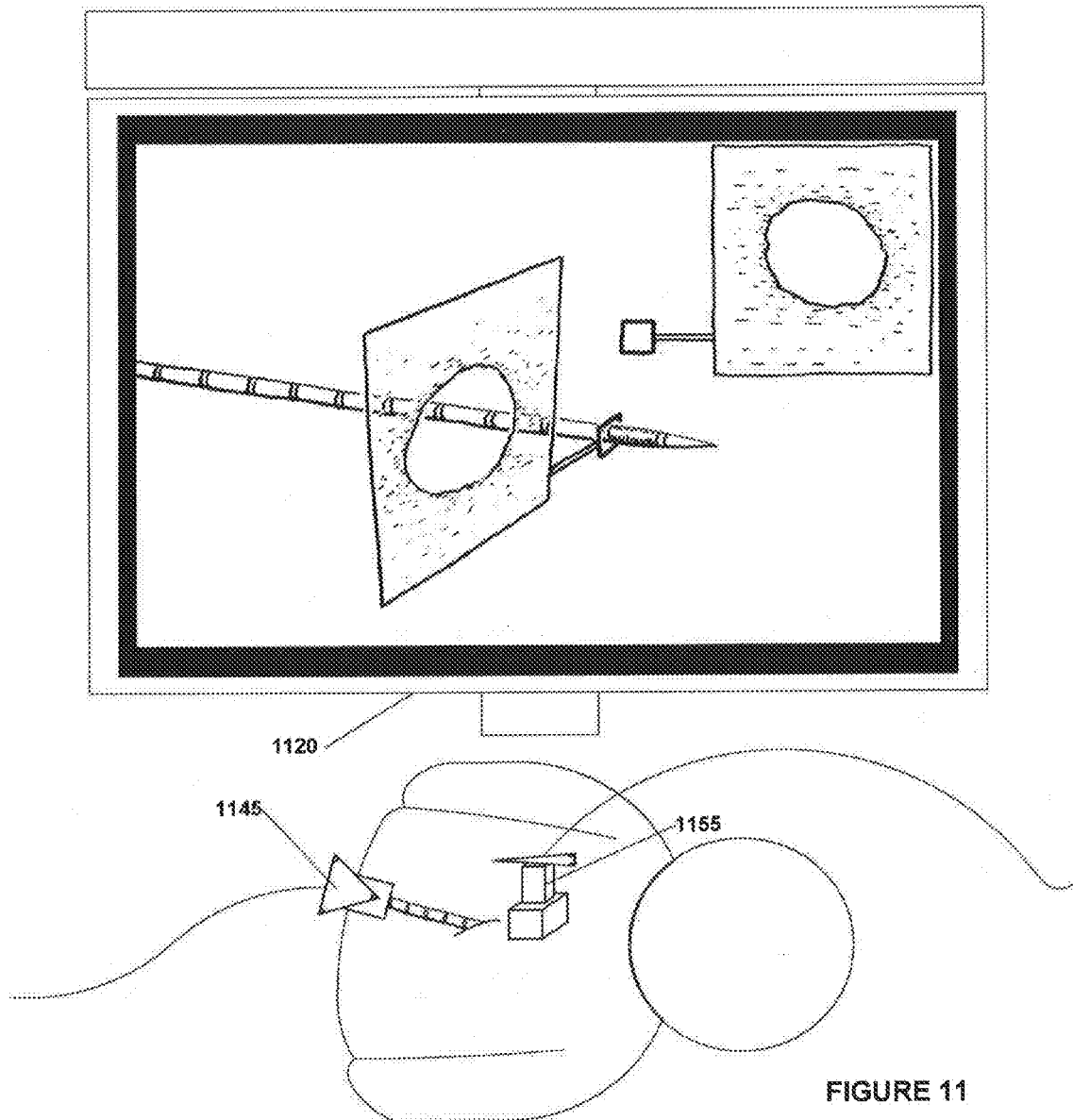


FIGURE 11

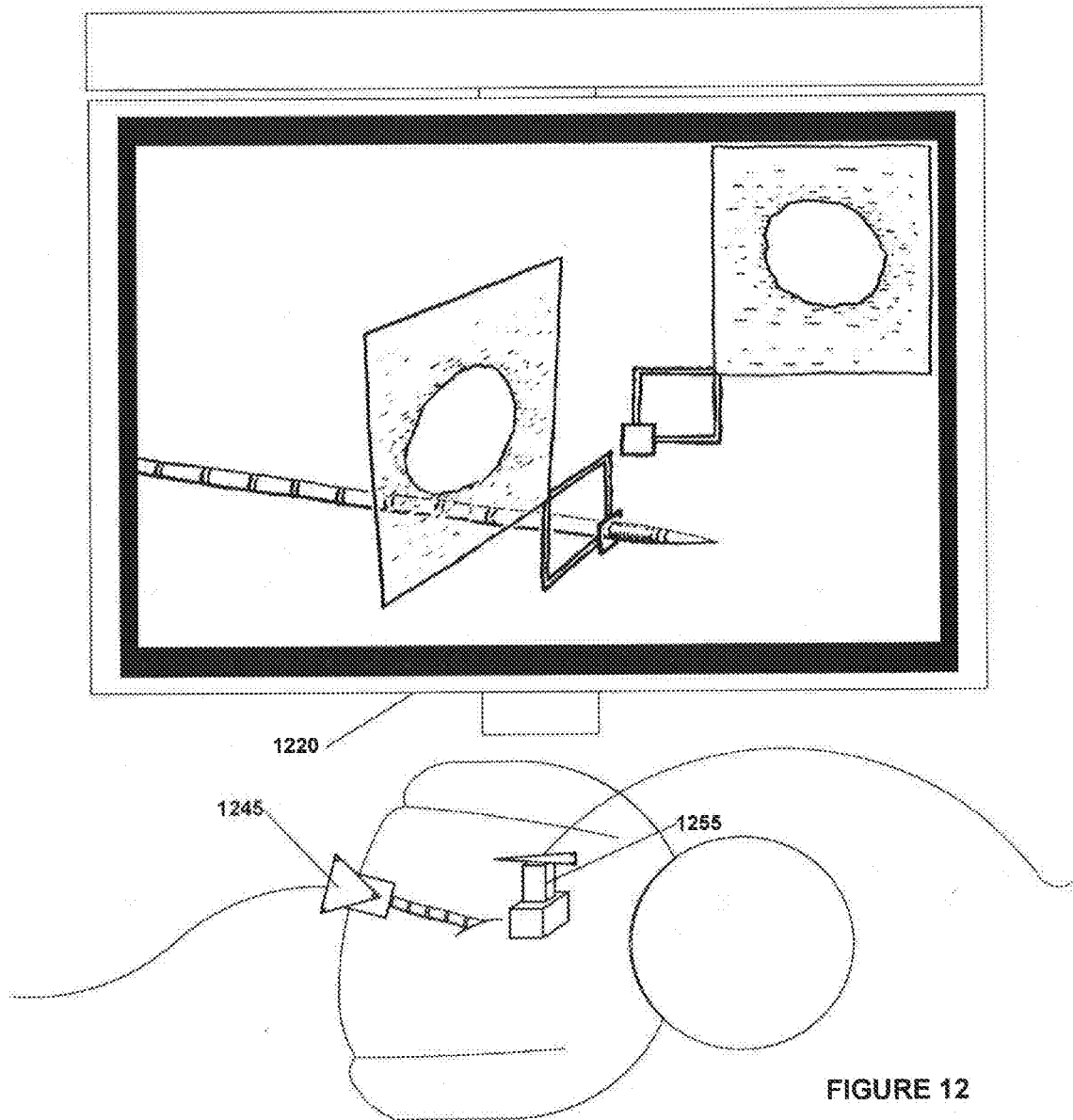
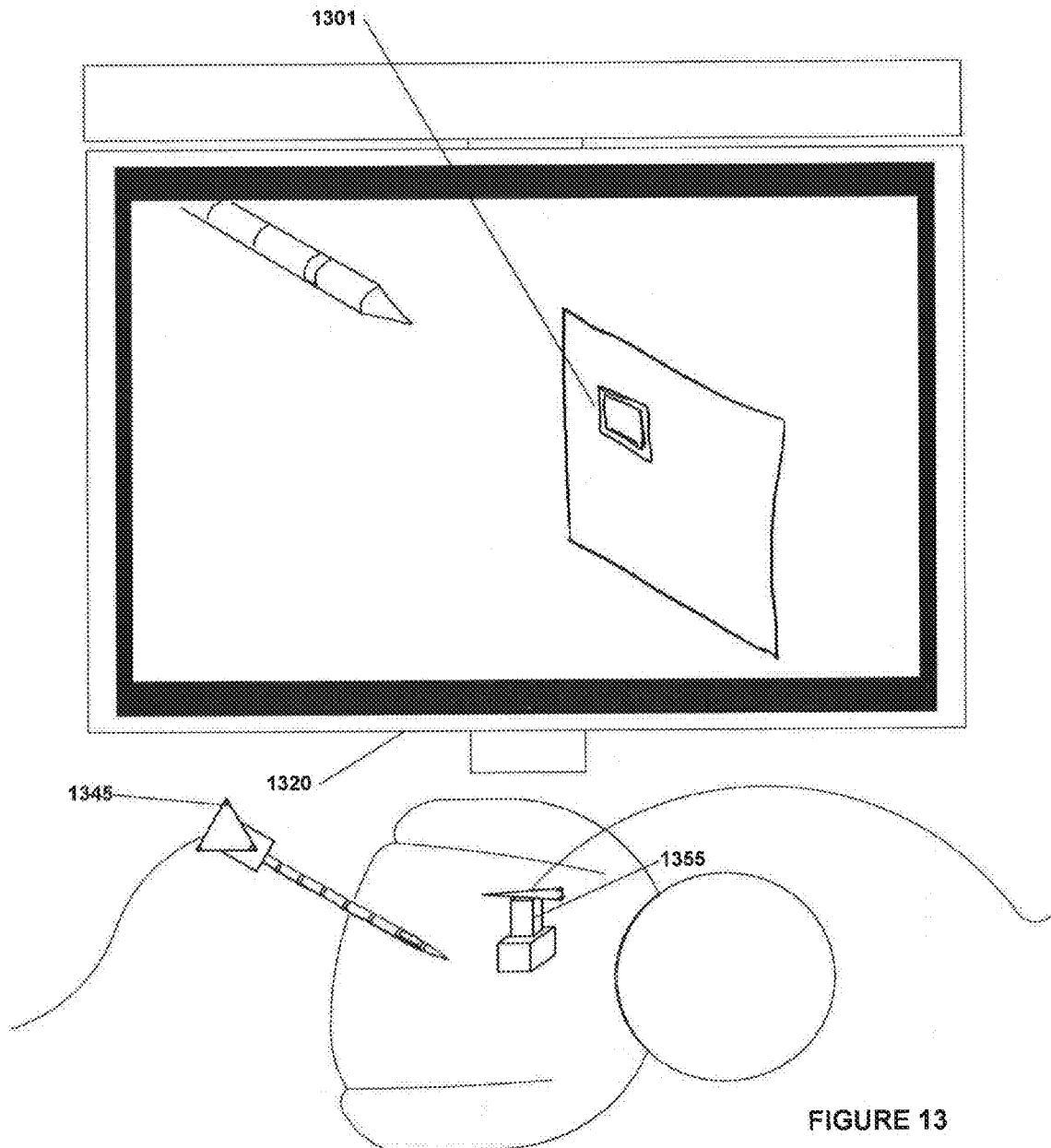
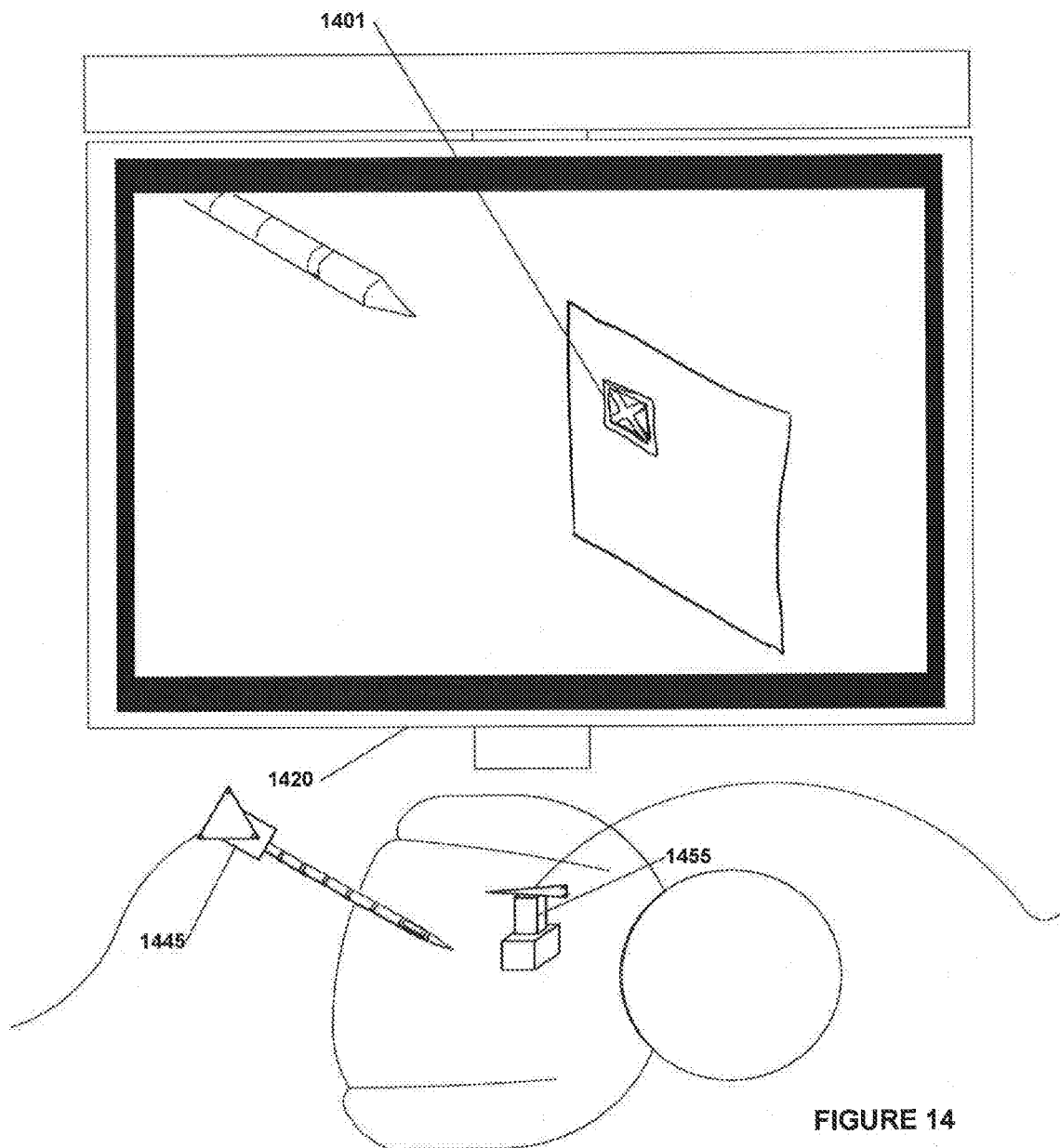
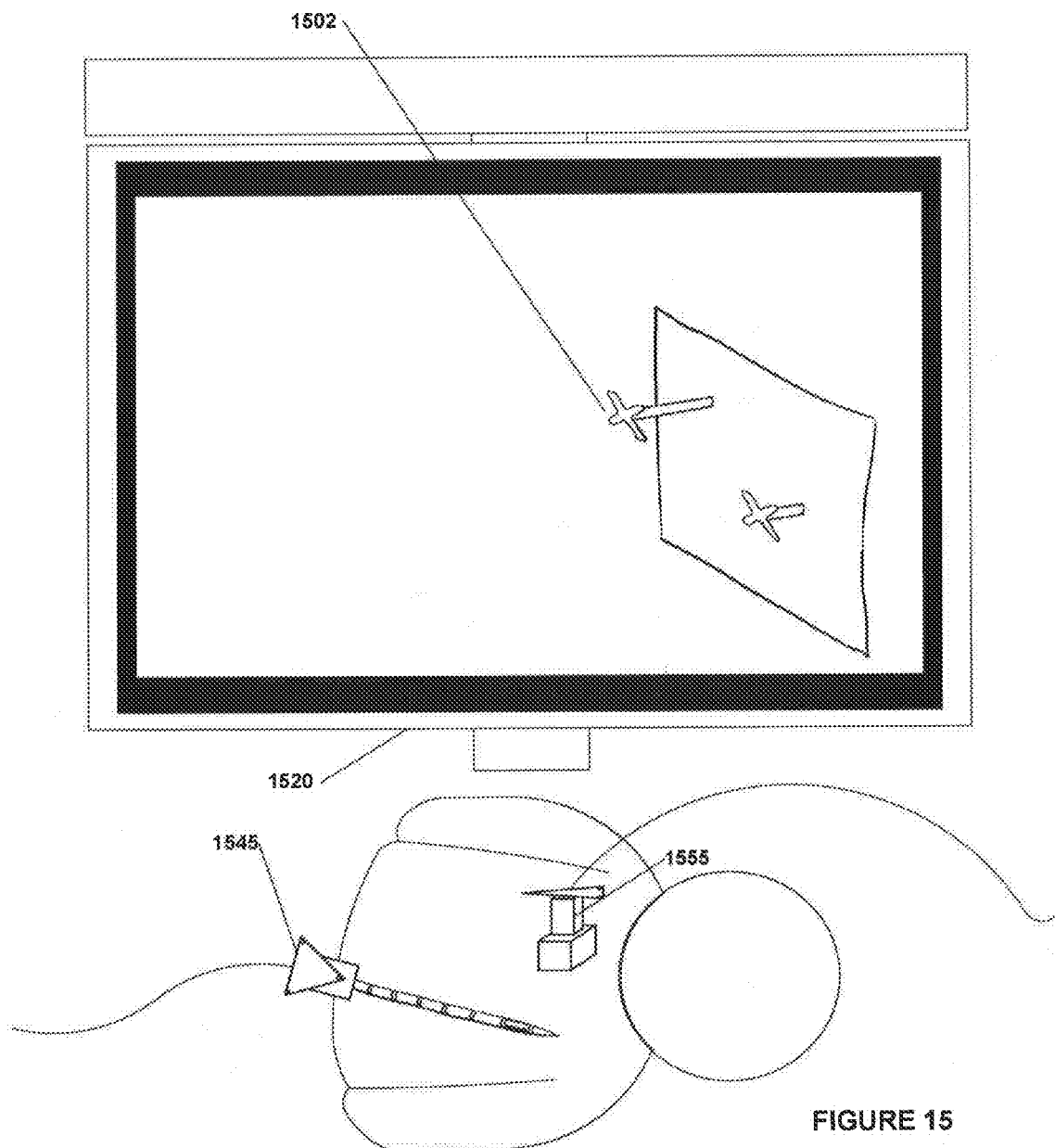


FIGURE 12







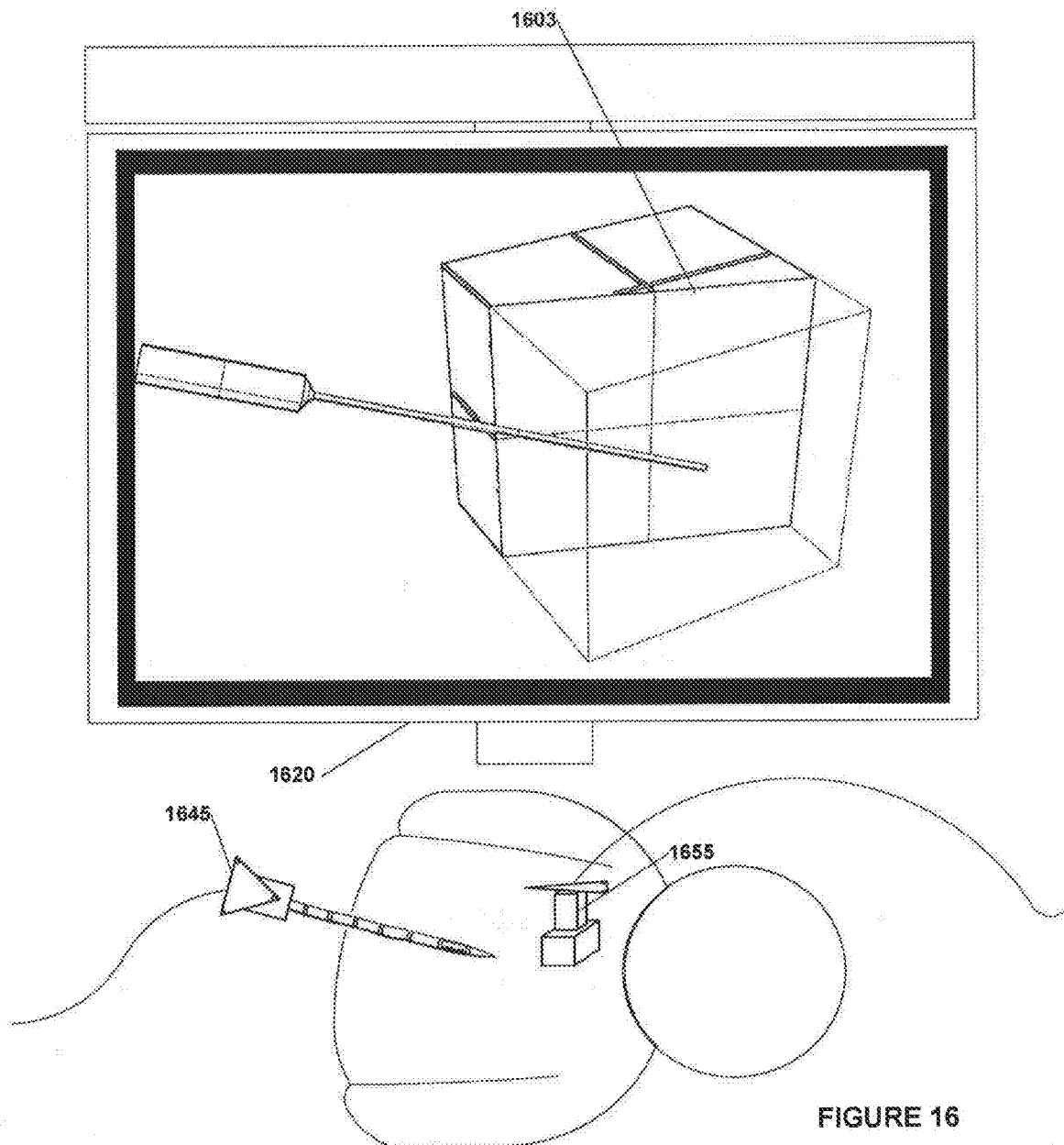


FIGURE 16

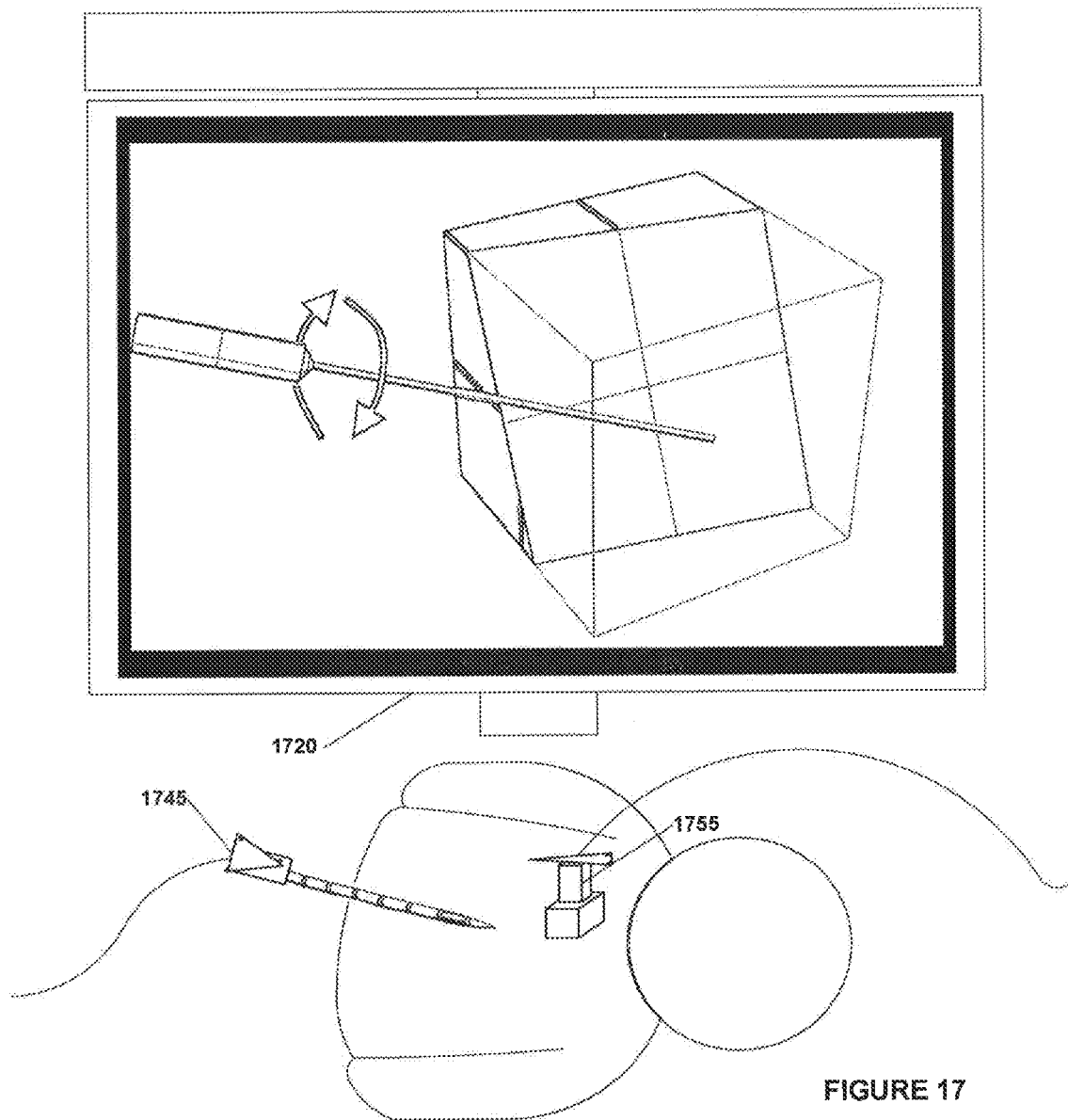


FIGURE 17

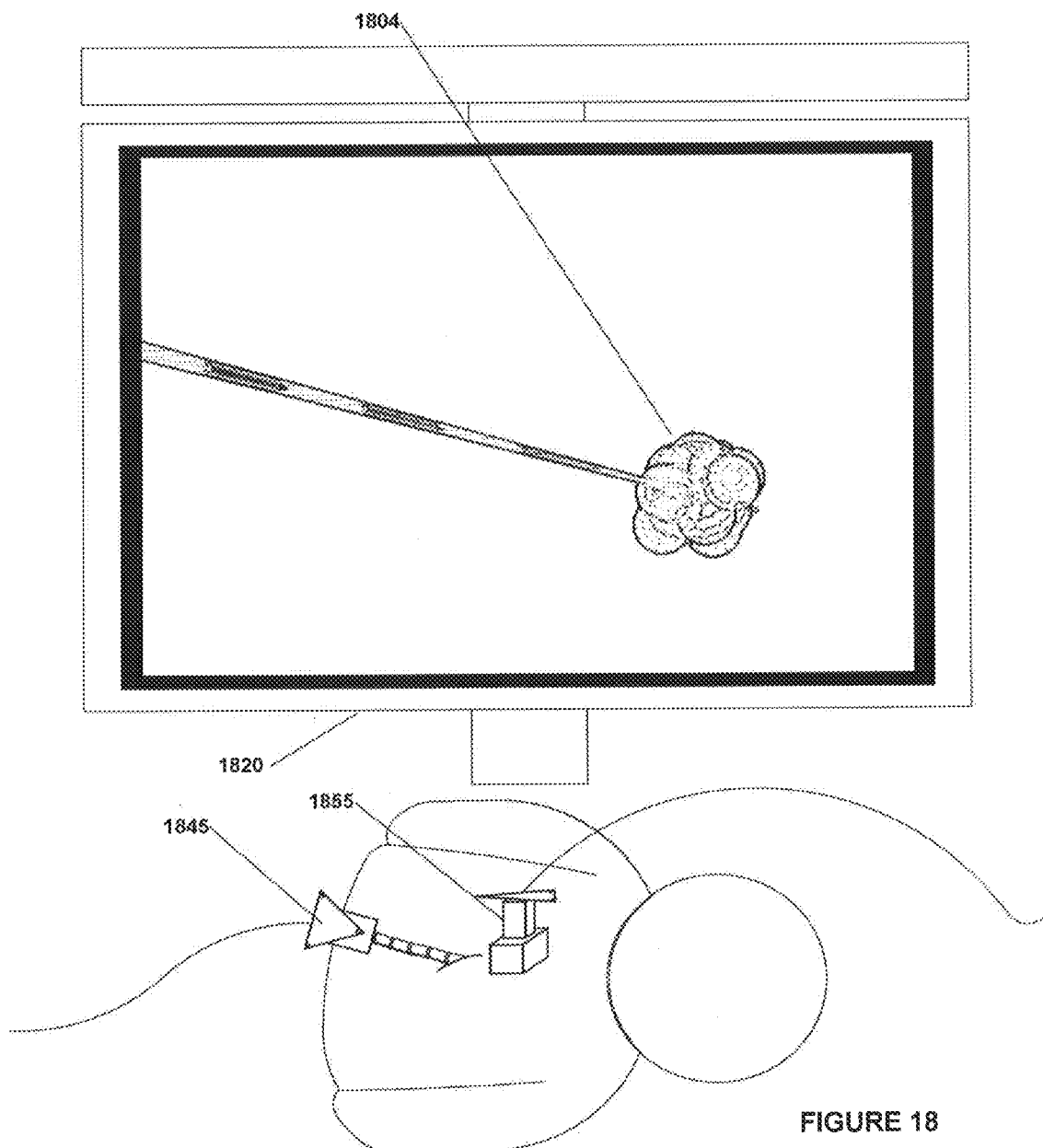


FIGURE 18

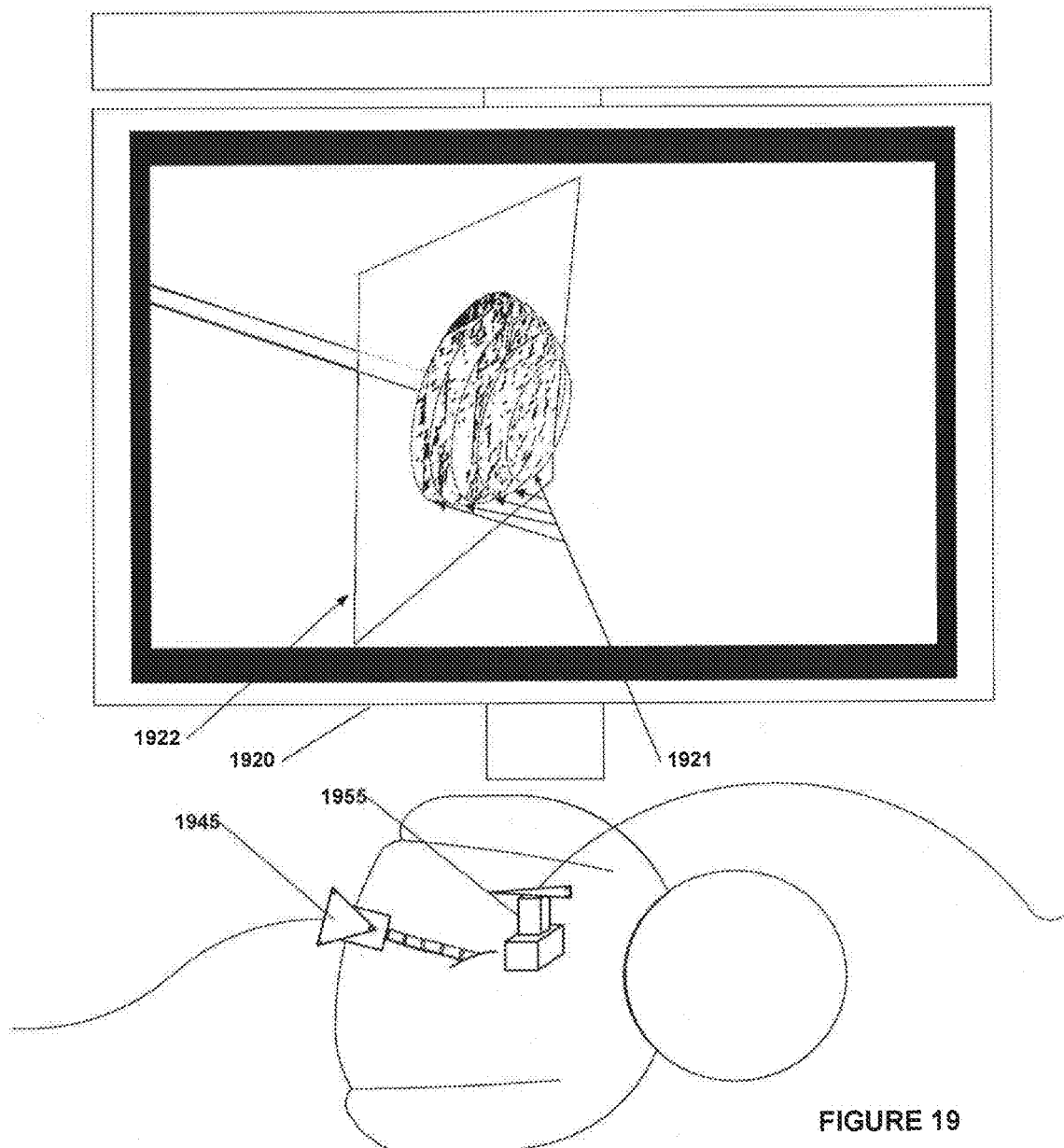


FIGURE 19

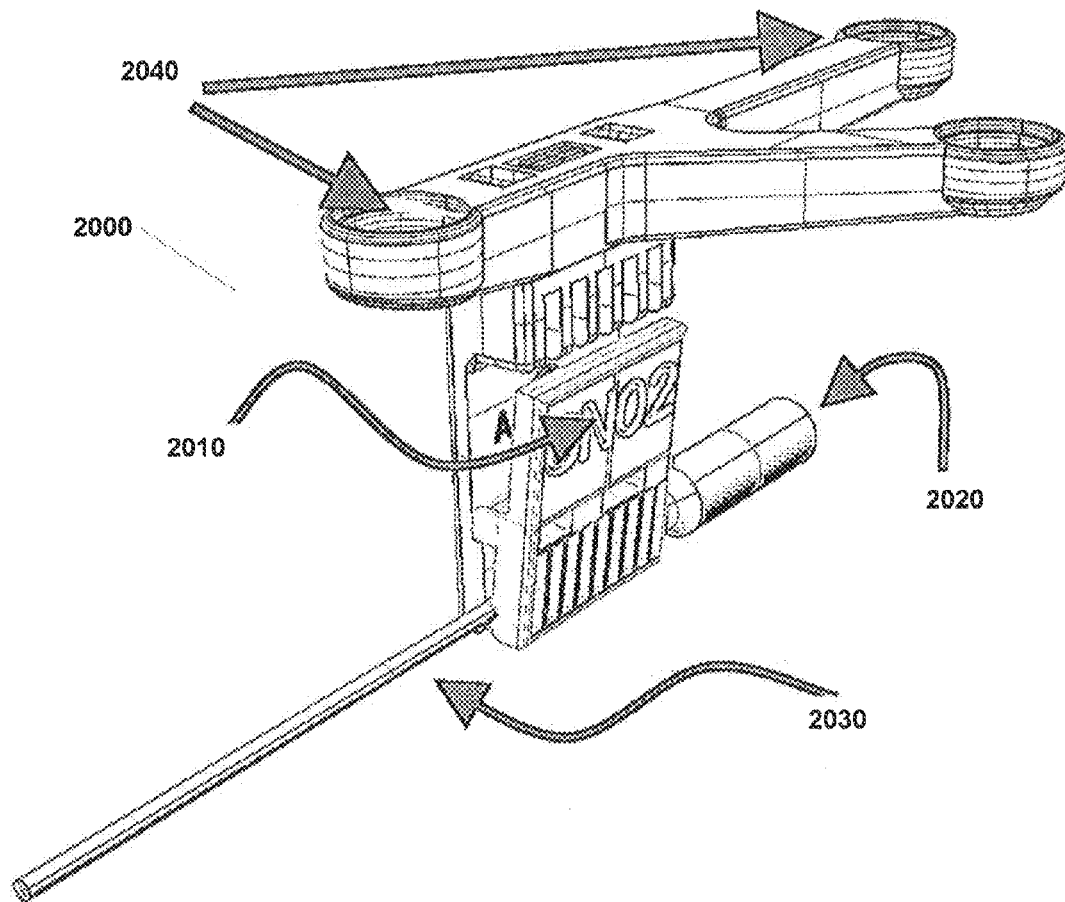


FIGURE 20

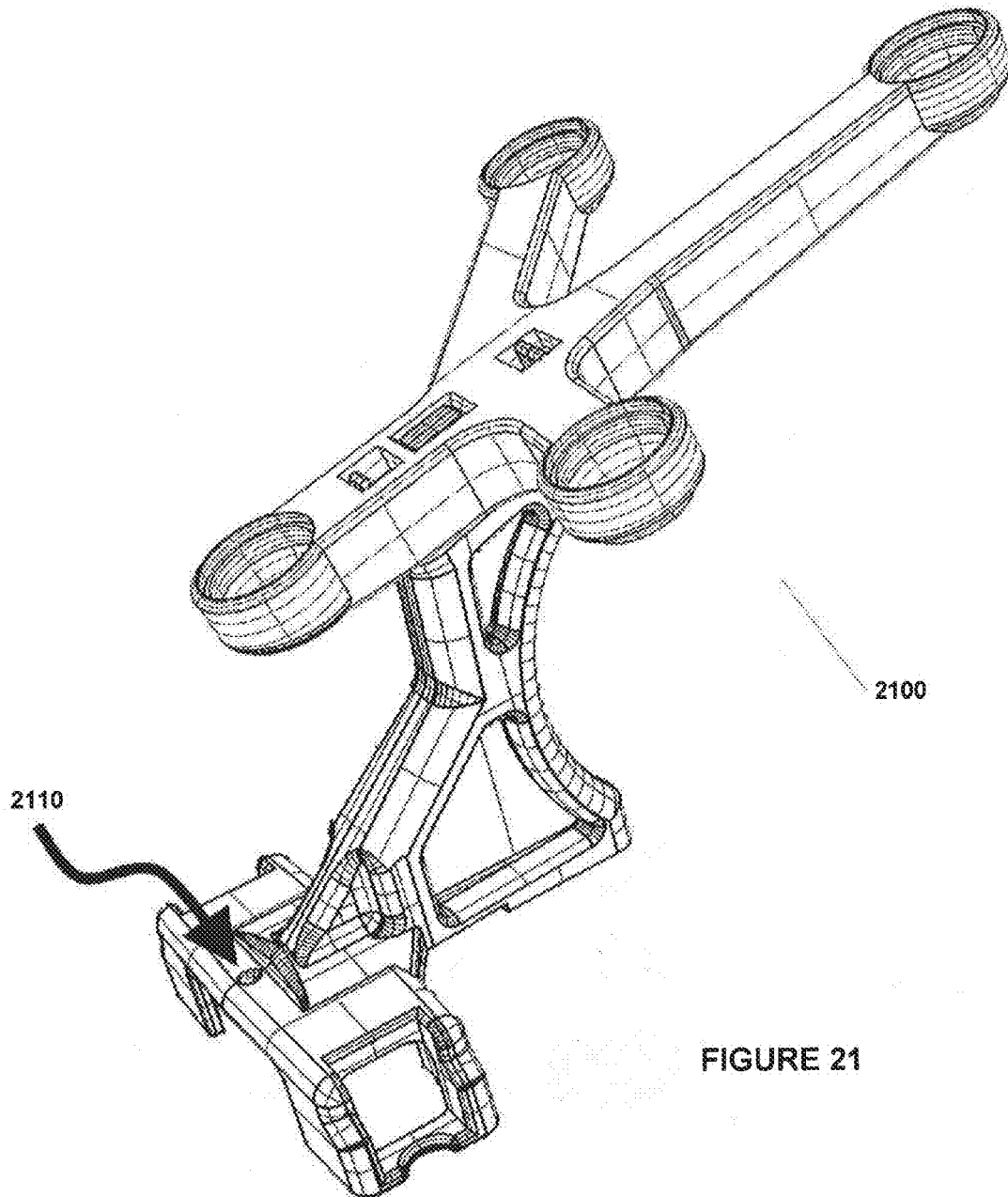
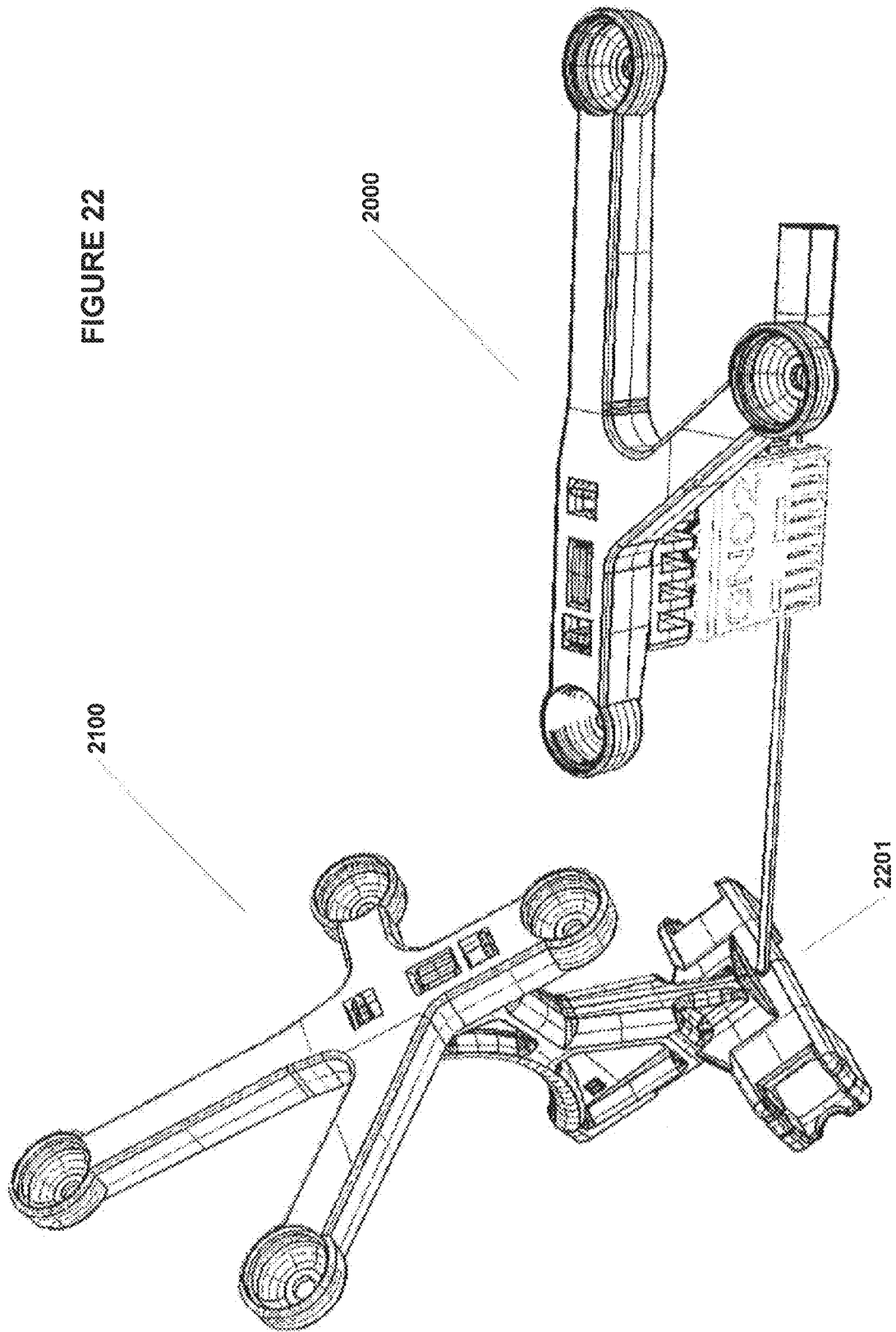


FIGURE 22



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SYSTEMS, METHODS, APPARATUSES, AND COMPUTER-READABLE MEDIA FOR IMAGE GUIDED SURGERY

CROSS-REFERENCE TO RELATED APPLICATION

This application is a continuation of U.S. application Ser. No. 12/703,118, filed on Feb. 9, 2010, which claims the benefit of U.S. Provisional Application No. 61/207,593, filed Feb. 17, 2009, U.S. Provisional Application No. 61/207,589, filed Feb. 17, 2009, and U.S. Provisional Application No. 61/207,592, filed Feb. 17, 2009, each of which is incorporated herein in its entirety for all purposes.

FIELD

The embodiments disclosed relate to computer-assisted surgery and more specifically related to systems, methods, apparatuses, and computer-readable media for image-guided surgery.

BACKGROUND

The past few decades have seen incredible development of technology and systems for computer assisted, image based, or image guided surgery. The advances in image guided surgery are tied in part to technological and scientific improvements in imaging and 3D computer graphics. For example, the early work of Mark Levoy, Turner Whitted, Richard Hol- loway, and Stephen Pizer in the late 1980s provided new 3D computer graphics rendering techniques, medical image shape detection, and head-mounted displays. These are some of the building blocks of later image-guided surgery systems built at the University of North Carolina in the mid 1990s and after.

Image guided surgery makes use of imaging to aid the surgeon to perform more effective or more accurate surgery. As merely one example of such image guided surgery, the use of ultrasound to guide needles being inserted into the liver for ablation are used by the surgeon to help guide the needle.

Current systems, however, have inadequate visualizations of image guidance data. This inadequate data may include the lack of useful information regarding an ablation needle and its potential effect on the procedure. Also, the equipment used for image guided surgery is typically difficult to calibrate. For example, each time a practitioner uses a new surgical instrument that must be optically tracked by an image guidance system, she must perform the following two steps. First, she must rigidly affix the tracking fiducials to the needle. This may involve tightening screws, or to threading a needle through a hole or tube. Second, she must measure the position of the tip of the needle, relative to the fiducials. This may involve manually measuring the surgical instrument length with a ruler, and then entering this information into a work- station; or using a dedicated calibration rig, and perform a lengthy (e.g., several minute) calibration process.

These problems and others are addressed by the systems, methods, devices and computer-readable media described herein.

SUMMARY

Presented herein are methods, systems, devices, and com- puter-readable media for image guided surgery. In some embodiments, a system may determine device type informa- tion for a first medical device; real-time emplacement infor-

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mation for the first medical device; and real-time emplace- ment information for a second medical device. The system may also determine the real-time relative emplacements of the first and second medical devices with the computer sys- tem and real-time prediction information for the first medical device. The image guidance system may then generate image guidance information based on the real-time relative emplacements of the first and second medical devices, the real-time prediction information for the first medical device, and data related to the second medical device. A graphical rendering of the image guidance information may be dis- played on one or more displays.

Numerous other embodiments are described throughout herein. Although various embodiments are described herein, it is to be understood that not necessarily all objects, advan- tages, features or concepts need to be achieved in accordance with any particular embodiment. Thus, for example, those skilled in the art will recognize that the invention may be embodied or carried out in a manner that achieves or opti- mizes one advantage or group of advantages as taught or suggested herein without necessarily achieving other objects or advantages as may be taught or suggested herein.

All of these embodiments are intended to be within the scope of the invention herein disclosed. These and other embodiments will become readily apparent to those skilled in the art from the following detailed description having refer- ence to the attached figures, the invention not being limited to any particular disclosed embodiment(s).

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 illustrates the display of 3D volumetric data as planar data along three axes.

FIG. 2 illustrates the display of 3D volumetric data as a 3D block of data.

FIG. 3A illustrates a first exemplary system for image guided surgery.

FIG. 3B illustrates a second exemplary system for image guided surgery.

FIG. 4 illustrates a first example of displaying image guid- ance data.

FIG. 5 illustrates a second example of displaying image guidance data.

FIG. 6 illustrates a third example of displaying image guid- ance data.

FIG. 7 illustrates a fourth example of displaying image guidance data.

FIG. 8 illustrates a fifth example of displaying image guid- ance data.

FIG. 9 illustrates a sixth example of displaying image guidance data.

FIG. 10 illustrates a seventh example of displaying image guidance data.

FIG. 11 illustrates an eighth example of displaying image guidance data.

FIG. 12 illustrates a ninth example of displaying image guidance data.

FIG. 13 illustrates a tenth example of displaying image guidance data.

FIG. 14 illustrates an eleventh example of displaying image guidance data.

FIG. 15 illustrates a twelfth example of displaying image guidance data.

FIG. 16 illustrates a thirteenth example of displaying image guidance data.

FIG. 17 illustrates a fourteenth example of displaying image guidance data.

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FIG. 18 illustrates a fifteenth example of displaying image guidance data.

FIG. 19 illustrates a sixteenth example of displaying image guidance data.

FIG. 20 illustrates a first calibration device for image guided surgery.

FIG. 21 illustrates a second calibration device for image guided surgery.

FIG. 22 illustrates an example of calibrating devices for image guided surgery.

DETAILED DESCRIPTION OF SPECIFIC EMBODIMENTS

Overview

In some embodiments, a system, such as depicted in FIGS. 3A and 3B, may track a surgical instrument, such as an ablation needle, and an imaging device, such as an ultrasound wand. In other embodiments, numerous other medical or surgical devices may be tracked, and the system may track three, four, or more of medical or surgical devices or medical devices. A “medical device” is a term that may include surgical devices and non surgical devices and all of those terms are broad terms and are intended to encompass their plain and ordinary meaning, including without limitation, ablation needles, scalpels, endoscopes, ultrasound wands, etc. Information about the surgical or medical devices may be predicted or determined and displayed by the system in 2D or 3D on a display visible to physician using the system. “Prediction information” is a broad term and is intended to encompass its plain and ordinary meaning, including without limitation, image guidance data, mathematical data, mathematical or 3D models related to a procedure, etc.

As an example embodiment, the system may determine or predict the intersection point of an ultrasound slice and the projection of an ablation needle. The system may also compute and display relative orientation information, and, in the case of collected 3D data, such as 3D ultrasound data, the system may segment and display the data in different manners, such as in 2D slices, 3D volumes, etc. This “extra” data displayed to the physician may be useful as it provides the physician with more information about the operation, the instruments, and/or data from the instruments.

Embodiments herein may be used for many kinds of needle-based medical procedures, including, but not limited to, radiofrequency-, cryo-, microwave-, laser-ablation of tumors, fibroids, lesions, etc, as well as biopsies, injections, central line placements, cyst aspirations, fluid drainings, lumpectomies, and guidance of wires and stents through blood vessels and ducts. Herein, the term needle to refer to any rigid needle-like object, such as an ablation antenna or probe, cannula, catheter, electro-cautery device, Bovie, laser waveguide, stent application device, etc. Needle may also refer to a non-rigid or nearly rigid version of the above. The system may also be used with non-needle devices such as scalpels, forceps, cutting loops on hysteroscopes, harmonic sheers, lasers (including CO₂ lasers), etc.

Some embodiments include tracking fixtures that may mount to surgical or medical devices, such as ablation needles, ultrasound wands, ultrasound probes, scalpels, etc. that allow for quicker attachment and easier tracking calibration for the devices. These embodiments may allow a physician to more quickly and easily start using the system.

Exemplary Systems

FIG. 3A illustrates a first exemplary system for image guided surgery. FIG. 3B illustrates a second exemplary system for image guided surgery. In many respects the embodi-

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ments illustrated by FIGS. 3A and 3B are similar and use similar numbering. Where the two are different, those differences are noted. The differences between the two figures may include that, in FIG. 3A, two position sensing units 310 and 340 are shown, whereas in FIG. 3B, only a single position sensing unit 310 is shown.

In some embodiments, position sensing units 310 and 340 may be tracking systems 310 and 340 and may track surgical instruments 345 and 355 and provide data to the image guidance unit 330. The image guidance unit 330 may process or combine the data and show image guidance data on display 320. This image guidance data may be used by a physician to guide a procedure and improve care. There are numerous other possible embodiments of system 300. For example, numerous of the depicted modules may be joined together to form a single module and may even be implemented in a single computer or machine. Further, position sensing units 310 and 340 may be combined and track all relevant surgical instruments 345 and 355, as discussed in more detail below and exemplified in FIG. 3B. Additional imaging units 350 may be included and combined imaging data from the multiple imaging units 350 may be processed by image guidance unit 330 and shown on display unit 320. Additionally, surgical systems 349 may also be included. Information about and from multiple surgical systems 349 and attached surgical instruments 345 may be processed by image guidance unit 330 and shown on display 320. These and other possible embodiments are discussed in more detail below.

In some embodiments, system 300 comprises a first position sensing unit 310, a display unit 320, and second position sensing unit 340 (if it is included) all coupled to image guidance unit 330. In some embodiments, first position sensing unit 310, display unit 320, and image guidance unit 330 are all physically connected to stand 370. Image guidance unit 330 may be used to produce images 325 that are displayed on display unit 320. The images 325 produced on display unit 320 by the image guidance unit 330 may be determined based on ultrasound or other visual images from first surgical instrument 345 and second surgical instrument 355. For example, if first surgical instrument 345 is an ablation needle 345 and second surgical instrument 355 is an ultrasound wand 355, then images 325 produced on display 320 may include the video from the ultrasound wand 355 combined with graphics, such as projected needle drive or projected ablation volume, determined based on the emplacement of ablation needle 345. If first surgical instrument 345 is an ultrasound wand 345 and second surgical instrument 355 is a laparoscopic camera 355, then images 325 produced on display 320 may include the video from the laparoscopic camera 355 combined with ultrasound data superimposed on the laparoscopic image. More surgical instrument may be added to the system. For example, the system may include an ultrasound wand, ablation needle, laparoscopic camera, cauterizer, scalpel and/or any other surgical instrument. The system may also include in the processing previously collected data, such as preoperative CT scans, X-Rays, MRIs, etc.

Emplacement as used herein may refer to pose, position, orientation, the combination or position and orientation, or any other appropriate location information. In some embodiments, the imaging data obtained from one or both of surgical instruments 345 and 355 may include other modalities such as a CT scan, MRI, open-magnet MRI, optical coherence tomography, positron emission tomography (“PET”) scans, fluoroscopy, ultrasound, or other preoperative or intraoperative 2D or 3D anatomical imaging data. In some embodiments, surgical instruments 345 and 355 may also be scalpels, implantable hardware, or any other device used in surgery.

Any appropriate surgical system **349** or imaging unit **350** may be attached to the corresponding medical instruments **345** and **355**.

As noted above, images **325** produced may also be based on live, intraoperative, or real-time data obtained using second surgical instrument **355**, which is coupled to second imaging unit **350**. As used herein, real-time data may be that data that is obtained at a frequency that would allow a surgeon to meaningfully interact with the data during surgery. For example, in some embodiments, real-time data may be a medical image of a patient that is updated one time per second. In some embodiments, real-time data may be ultrasound data that is updated multiple times per second. Second surgical instrument **355** may be coupled to second position sensing unit **340**. Second position sensing unit **340** may be part of imaging unit **350** or it may be separate. Second position sensing unit **340** may be used to determine the emplacement of second surgical instrument **355**. In some embodiments, first and/or second position sensing units **310** and/or **340** may be magnetic trackers and magnetic may be coils coupled to surgical instruments **345** and/or **355**. In some embodiments, first and/or second position sensing units **310** and/or **340** may be optical trackers and visually-detectable fiducials may be coupled to surgical instruments **345** and/or **355**.

Images **325** may be produced based on intraoperative or real-time data obtained using first surgical instrument **345**, which is coupled to first surgical system **349**. In FIGS. 3A and 3B, first surgical system **349** is shown as coupled to image guidance unit **330**. The coupling between the first surgical system **349** and image guidance unit **330** may not be present in all embodiments. In some embodiments, the coupling between first surgical system **349** and image guidance unit **330** may be included where information about first surgical instrument **345** available to first surgical system **349** is useful for the processing performed by image guidance unit **330**. For example, in some embodiments, first surgical instrument **345** is an ablation needle **345** and first surgical system **349** is an ablation system **349**. In some embodiments, it may be useful to send a signal about the relative strength of planned ablation from ablation system **349** to image guidance unit **330** in order that image guidance unit **330** can show a predicted ablation volume. In other embodiments, first surgical system **349** may not be coupled to image guidance unit **330**. Example embodiments including images and graphics that may be displayed are included below.

In some embodiments, first position sensing unit **310** tracks the emplacement of first surgical device **345**. First position sensing unit **310** may be an optical tracker **310** and first surgical device **345** may have optical fiducials attached thereto. The emplacement of optical fiducials may be detected by first position sensing unit **310**, and, therefrom, the emplacement of first surgical device **345** may be determined.

In various embodiments, as depicted in FIG. 3B, a single position sensing unit **310** may track both first medical device **345** and second medical device **355**. In FIG. 3B, in some embodiments, position sensing unit **310** is a magnetic tracker and is mounted below a surgical table **380**. Such an arrangement may be useful when the tracking volume of the position sensing unit **310** is dependent on the location of the position sensing unit, as with many magnetic trackers. Magnetic tracking coils may be mounted in or on the medical devices **345** and **355**.

In some embodiments, either or both of the first position sensing unit **310** and the second position sensing unit **340** may be an Ascension Flock of Birds, Nest of Birds, driveBAY, medSAFE, trakSTAR, miniBIRD, MotionSTAR, pciBIRD, or Calypso 4D Localization System and tracking units

attached to the first and or second surgical or medical devices **345** and **355** may be magnetic tracking coils. In some embodiments, either or both of the first position sensing unit **310** and the second position sensing unit **340** may be an Aurora® Electromagnetic Measurement System using sensor coils for tracking units attached to the first and or second surgical devices **345** and **355**. In some embodiments, either or both of the first position sensing unit **310** and the second position sensing unit **340** may also be an optical 3D tracking system using fiducials. Such optical 3D tracking systems may include the NDI Polaris Spectra, Vicra, Certus, PhaseSpace IMPULSE, Vicon MX, InterSense IS-900, NaturalPoint OptiTrack, Polhemus FastTrak, IsoTrak, or Claron Micon-Tracker2. In some embodiments, either or both of position sensing units **310** and **340** may be attached to or affixed on the corresponding surgical device **345** and **355**. In some embodiments, the position sensing units, **310** and **340**, may include sensing devices such as the HiBall tracking system, a GPS device or signal emitting device that would allow for tracking of the position and, optionally, orientation of the tracking unit. In some embodiments, a position sensing unit **310** or **340** may be affixed to either or both of the surgical devices **345** and **355**. The surgical devices **345** or **355** may be tracked by the position sensing units **310** or **340**. A world reference, such as the display **320** may also be tracked by the position sensing unit **310** or **340** in order to determine the emplacements of the surgical devices **345** and **355** with respect to the world. Devices **345** and **355** may also include or have coupled thereto one or more accelerometers, which may be used to estimate movement, position, and location of the devices.

In some embodiments, the display unit **320** displays 3D images to a physician. Stereoscopic 3D displays separate the imagery shown to each of the user's eyes. This can be accomplished by a stereoscopic display, a lenticular auto-stereoscopic display, or any other appropriate type of display. The display **320** may be an alternating row or alternating column display. Example alternating row displays include the Miracube G240S, as well as Zalman Trimon Monitors. Alternating column displays include devices manufactured by Sharp, as well as many "auto-stereoscopic" displays (e.g., Philips). Display **320** may also be a cathode ray tube. Cathode Ray Tube (CRT) based devices, may use temporal sequencing, showing imagery for the left and right eye in temporal sequential alternation; this method may also be used by newer, projection-based devices, as well as by 120-Hz-switchable liquid crystal display (LCD) devices.

In some embodiments, a user may wear a head mounted display in order to receive 3D images from the image guidance unit **330**. In such embodiments, a separate display, such as the pictured display unit **320**, may be omitted. The 3D graphics may be produced using underlying data models, stored in the image guidance unit **330** and projected onto one or more 2D planes in order to create left and right eye images for a head mount, lenticular or other 3D display. The underlying 3D model may be updated based on the relative emplacements of the various devices **345** and **355**, as determined by the position sensing unit(s), and/or based on new data associated with the devices **345** and **355**. For example, if the second device is an ultrasound wand **355**, then the underlying data model may be updated to reflect the most recent ultrasound image. If the first device **345** is an ablation needle, then the underlying model may be updated to reflect any changes related to the needle, such as power or duration information. Any appropriate 3D graphics processing may be used for rendering including processing based on OpenGL, Direct3D, Java 3D, etc. Whole, partial, or modified 3D graphics packages may also be used, such packages including 3DS

Max, SolidWorks, Maya, Form Z, Cybermotion 3D, or any others. In some embodiments, various parts of the needed rendering may occur on traditional or specialized graphics hardware. The rendering may also occur on the general CPU, on programmable hardware, on a separate processor, be distributed over multiple processors, over multiple dedicated graphics cards, or using any other appropriate combination of hardware or technique.

There are numerous other examples of image guidance systems which may use, incorporate, support, or provide for the techniques, methods, processes, and systems described herein, such as the 3D computer-graphics-based assigned to InnerOptic Technologies, Inc. that provides for displaying guidance data from multiple sources, U.S. application Ser. No. 11/833,134, filed Aug. 2, 2007, the contents of which are incorporated herein in their entirety for all purposes.

Image Guidance Processes and Data

Depicting Surgical Instruments

Previous systems do not provide satisfactory image guidance data. It can often be difficult to discern the content of a 3D scene from a 2D depiction of it, or even from a 3D depiction of it. Therefore, various embodiments herein provide image guidance that can help the doctor better understand the scene, relative emplacements or poses of object in the scene and thereby provide improved image guidance. FIG. 4 illustrates an image 401 of an exemplary surgical instrument 445 being displayed on a screen 420. In this case, the surgical instrument displayed is an ablation needle 445. Also depicted is the wire 446 connecting the ablation needle to an ablation system. Some models of needles have markings such as bands around the shaft (to indicate distance along the shaft), and a colored region near the tip to indicate where the radio frequency or microwave energy is emitted from in the case of an ablation probe. Physicians performing needle procedures are often familiar with these markings and may use them to help understand the spatial relationship between the needle and anatomy. In some embodiments, the make and model of the needle 445 is known to the image guidance system and the needle displayed (401) in display 420 may resemble needle 445. The features of needles that may be rendered in the scene include the overall shape (diameter, cross sectional shape, curvature, etc.), color, distance markers, visuals or echogenic fiducial markers, the state of deployable elements such as tines, paddles, anchors, resection loops, stiffening or steerable sleeves, temperature, radiation, light or magnetic field sensors, lens, waveguides, fluid transfer channels, and the like.

The type of needle being used may be input into the image guidance system, may be a system default, may be detected by a camera or other device, may be received as data from an attached medical device, such as surgical system 349 in FIGS. 3A and 3B, or the information may be received in any other appropriate manner. Making the surgical instrument displayed on display 420 resemble the surgical instrument 445 may help physicians associate the image guidance data with the real world and may provide more familiar guidance information to a physician, thereby further aiding the physician in the guidance task. For example, the surgeon may see the familiar markings on the needle being displayed on the display 420 and therefore be familiar with the distance and relative placement of the displayed needle with respect to other data, such as a tumor seen in an ultrasound (not depicted in FIG. 4). This knowledge of relative placement of items being displayed may help the surgeon get the needle into place.

Consider an embodiment in which the image in the display 420 has a needle depicting the portion of the needle that will

perform the ablation, for example, the portion that emits the radio or microwave energy. If the display 420 also includes ultrasound data, then the doctor may be able to find the tumor she wishes to ablate by moving the ultrasound wand around until she spots the tumor. In various embodiments, she will be able to see the displayed ultrasound data and its location relative to the displayed needle with the markings. She can then drive the needle until she sees, on display 420, that the emitter-portion of the needle encompasses the tumor in the ultrasound, also seen on display 420. When she activates the ablation, she can then be much more certain that she has ablated the correct portion of the tissue. Various embodiments of this are discussed more below.

As another example, consider the physical markings that may be on the instruments themselves. These markings can help orient a physician during use of the instrument. In some embodiments, the image guidance unit may represent these markings in the images displayed in the display. For example, certain ultrasound transducers are built with an orientation mark (e.g., a small bump) on one side of the transducing array. That mark may also be shown in the ultrasound image on the scanner's display, to help the physician understand where the scanned anatomical structures shown on screen are located under the transducer, inside the patient. In some embodiments, the image guidance system may display a symbolic 3D representation of the orientation mark both next to the motion-tracked ultrasound slice (e.g., moving with the displayed ultrasound slice) and next to the 2D ultrasound slice also displayed by the IVS. An example of this is displayed in FIG. 7, where a small rectilinear volume corresponding to a feature on an ultrasound wand is shown both in proximity to the ultrasound slice displayed in 3D and the ultrasound slice displayed as a 2D image.

Other embodiments will track and display other types of instruments and their features. For example, a surgeon may want to track one or more of a scalpel, a cauterizer (including an electrocauterizer and Bovie's), forceps, cutting loops on hysteroscopes, harmonic sheers, lasers (including CO₂ lasers), etc. For example, in various embodiments, the following devices may be tracked and various aspects of their design displayed on display 420:

- Olympus™ OES Pro Hystero-Resectoscope, SonoSurg Ultrasonic Surgical System
- Olympus™ GF-UC 160 Endoscope
- Wallus™ Embryo Transfer Catheter
- AngioDynamics® NanoKnife™, VenaCure™ laser, StarBurst, UniBlade, Habib® Resector
- Bovie® Electrodes
- Covidien Evident™, Cool-Tip™ Ablation Antennas, Opti4™ Electrodes
- Microsulis MEA (microwave endometrial ablation), Acculis
- Halt™ Medical System
- Optimed BigLumen Aspiration Catheter
- Optimed Optipure Stent
- Central venous catheterization introducer needle (such as those made by Bard and Arrow)

Once tracked, a physician may be able to see image guidance data on display 420 that will allow her to know the relative pose, location, or emplacement of the tracked instrument(s) with respect to one another or with respect to imaging data and will be able to see, on display 420, the features of the instrument rendered in the scene.

Depicting Ablation Volume and Other Instrument Information

Various embodiments of the systems herein will depict as part of the image guidance data information related to the

surgical instruments. For example, in some embodiments, an image guidance system such as the systems of FIG. 3A or 3B may illustrate an expected spherical ablation volume. For example, FIG. 5 shows an ablation needle 545 which has a darkened portion that indicates where the radio frequency or microwave energy for ablation will be emitted. In some embodiments, an image guidance system may display on display 520 the expected ablation volume 502. The ablation volume 502 may be shown as a transparent volume, a wire-frame volume (depicted in FIG. 5), as a point cloud of various densities, as an outline, as a volume, or in any other appropriate manner.

For some ablation needles, the expected volume of ablated tissue is neither spherical nor centered at the tip of the needle. For example: a Covidien surgical microwave needle has an ellipsoidal ablation volume; a Covidien Evident transcatheter microwave needle has a teardrop-like ablation volume; RFA Medical's bipolar ablation system uses two needles simultaneously, where each needle has paddles that deploy after the needle is inserted inside the tissue (which one may equate to a canoe's oar). In some embodiments, the ablation volume for such a needle is, to a first approximation, a volume that lies directly between the paddles of the two needles.

The position and orientation of the volume may be specified by the placement of a tracked needle, such as needle 545 in FIG. 5. In some embodiments, with single needle ablation systems, the volume's approximate size (e.g., girth and length, if ellipsoidal) may be either specified by the physician, or automatically computed by the guidance system. The ablation volume may be based on numerous parameters such as the needle make and model, power and duration settings of the microwave or radio frequency generator, measured or estimated temperature and impedance of the target tissue or other tissue information, a formula, a look-up-table, fixed or default values, or based on any other appropriate available information.

Other instrument information may also be depicted. For example, if a cauterizer is tracked as part of an image guidance system, then the cauterization volume may be determined or estimated and that volume may be displayed. If a laser is tracked as part of the image guidance system, then the projected laser path may be determined or estimated and displayed.

Depicting Needle Drive Projection and Other Prediction Information

In certain procedures, there may be prediction information related to the surgical instruments. In the context of scalpel movement, this may be the location that the scalpel will hit if a physician continues to move the scalpel in a particular direction. In the context of ablation, this may be the projected needle placement if it is driven along its central axis. FIG. 6 illustrates both an ablation volume for an ablation needle and a projected needle drive 603. If a physician is driving an ablation needle 645 into tissue (not pictured), then she may want to know where the needle will be driven. In some embodiments, the projected drive of a needle 645 may be depicted on the display 620 and may show the physician the projected path 603 that the needle will take if it is driven along its central axis.

In some embodiments, in order to aid the physician in placing or orienting a needle 645, an image guidance system, such as that depicted in FIG. 3A or FIG. 3B, may draw a number of rings about the axis of the needle shaft, extrapolated beyond its tip, as depicted in FIG. 6. A physician may view and manipulate the position and orientation of the needle 645 and its expected drive projection (via its displayed projected trajectory) before it enters the patient's tissue. In

some embodiments, this is accomplished by the doctor positioning the virtual rings in the drive projection such that they are co-incident (or pass through) the ultrasound representation of a target, such as a tumor that the doctor has spotted in the ultrasound. This may allow the physician to verify that the needle 645 is properly aimed at the target and can drive the needle 645 forward into the tissue such that it reaches its desired target or destination. For example, if the doctor spotted a tumor in the ultrasound image (not pictured in FIG. 6), she may be able to align the ablation needle 645 such that the drive projection rings on display 620 intersected or otherwise indicated that the needle, if driven straight, will reach the tumor.

The rings may be spaced at regular (e.g., 0.5, 1, or 2 cm) intervals to provide the physician with visual cues regarding the distance from the needle tip to the targeted anatomy. In some embodiments, the spacing of the rings may indicate other aspects of the data, such as the drive speed of the needle, the density of the tissue, the distance to a landmark, such as the ultrasound data, or any other appropriate guidance data or property. In some embodiments, the rings or other trajectory indicator may extend beyond the needle tip, by a distance equal to the length of the needle-shaft. This way, the user knows if the needle is long enough to reach the target—even before the tip enters the patient. That is, in some embodiments, if the rings do not reach the target with the tip still outside the body, then the tip won't reach the target even when the entire length shaft is inserted into the body.

Other display markers may be used to show trajectory, such as a dashed, dotted, or solid line, transparent needle shaft, point cloud, wire frame, etc. In some embodiments, three-dimensional rings may be used and provide depth cues and obscure little of the ultrasound image. Virtual rings or other virtual markers may be displayed semi-transparently, so that they obscure less of the ultrasound image than an opaque marker would.

Other prediction information may also be displayed. For example, if a scalpel is being tracked by the image guidance system, then a cutting plane corresponding to the scalpel may be displayed (not pictured). Such a cutting plane may be coplanar with the blade of the scalpel and may project from the blade of the scalpel. For example, the projected cutting plane may show where the scalpel would cut if it were the doctor were to advance the scalpel. Similar prediction information may be estimable or determinable for cauterizers, lasers, and numerous other surgical instruments.

Depicting Combinations of Graphics

As discussed herein, when there are multiple instruments or devices being used in a procedure, images, graphics, and data associated with the multiple instruments may be displayed to the physician. In some embodiments, as depicted in FIG. 7, when there are two devices 745 and 755 being used and tracked in a procedure, data, images, and graphics associated with those two images may be combinable and may be displayed on the same display. FIG. 7 depicts an ablation needle 745 and an ultrasound wand 755 being used during a procedure. Data associated with each of the devices 745 and 755 are displayed on the display 720.

The data from two or more devices may be combined and displayed based on their relative emplacements or poses. For example, an ultrasound image 704 may be displayed with respect to an ablation needle on a display 720 in a manner that estimates the relative emplacements or poses of an ultrasound wand 755 and ablation needle 745. This is depicted in FIG. 7. In FIG. 7, the graphics associated with the ablation needle 745, including the ablation volume and projected drive location are shown spatially located with the oriented planar

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ultrasound image on display **720**. In this image **704**, a tumor appears in the ultrasound image and the ablation needle is shown driven through the tumor. The ablation volume estimates where ablation would occur if it tissue were ablated at that time. The physician can see that the ablation volume appears to cover the tumor displayed in the ultrasound image.

Various embodiments include other combinations of graphics. For example, in some embodiments, data related to a single surgical instrument (such as an ablation needle, ultrasound wand, etc.) may be presented in more than one manner on a single display. Consider an embodiment in which device **745** is an ablation needle and device **755** is an ultrasound transducer. If a physician orients ultrasound transducer **755** such that it is perpendicular to the monitor, the 3D view of the ultrasound image would show only the edge and the ultrasound image would not be visible. In some embodiments, the image guidance system could track the physician's head using a position sensor, such as first and/or second position sensing units **310** and/or **340** of FIG. 3A or FIG. 3B. The physician then may be able to move her head to the side, so that she sees the ultrasound image from a different perspective.

In some embodiments, the image guidance system can constantly display an additional 2D view of the ultrasound image **705** (in screen space), simultaneous to the 3D depiction of the procedure, so that the ultrasound image is always visible, regardless of the orientation in which the physician holds the transducer. This is illustrated in FIG. 7. This display of the ultrasound data may be similar to what a physician is accustomed to seeing with traditional ultrasound displays. This may be useful to provide the physician with imaging to which she is accustomed and allows a physician to see the ultrasound data regardless of the then-current orientation of the ultrasound wand with respect to the user.

In some embodiments, the 2D view **705** of an ultrasound image is depicted in the upper right corner of the monitor (though it can be placed in any corner). The guidance system can automatically (and continually) choose a corner in which to render the 2D view of the ultrasound image, based on the 3D position of the surgical instruments in the rendered scene. For example, in FIG. 7, ablation needle **745** may be held in the physician's left hand and the needle shaft is to the left of the 3D ultrasound image slice, so that the 2D ultrasound image **705** in the upper right corner of display **720** does not cover any of the 3D features of the needle (or vice-versa). If the needle were held in the physician's right hand, the virtual needle shaft would appear on the right side. To prevent the 2D ultrasound image in the corner of display **720** from covering the needle shaft, the system can automatically move it to a corner that would not otherwise be occupied by graphics or data.

In some embodiments, the system attempts to avoid having the 2D ultrasound image quickly moving among corners of the display in order to avoid overlapping with graphics and data in the display. For example, a function f may be used to determine which corner is most suitable for the 2D ultrasound image to be drawn in. The inputs to f may include the locations, in the screen coordinate system, of the displayed needle tip, the corners of the 3D ultrasound image, etc. In some embodiments, f 's output for any given point in time is independent of f 's output in the previous frames, which may cause the ultrasound image to move among corners of the display rapidly. In some embodiments, the image guidance system will filter f 's output over time. For example, the output of a filter g , for any given frame, could be the corner which has been output by f the most number of times over the last n frames, possibly weighting the most recent values for f most heavily. The output of the filter g may be used to deter-

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mine in which corner of display **720** to display the 2D ultrasound image and the temporal filtering provided by g may allow the 2D ultrasound image display to move more smoothly among the corners of the display **720**.

In some embodiments, other appropriate virtual information can be overlaid on the 2D ultrasound image as well. Examples include: an indication of the distance between the needle's tip and the point in the plane of the ultrasound image that is closest to the needle tip; the cross section or outline of the ablation volume that intersects with the ultrasound slice; and/or the intersection point, box, outline, etc. between the needle's axis and the ultrasound image plane.

Representing Spatial Relationships

At times, when three dimensional relationships are depicted in 2D, or even in 3D, it may be difficult to gauge the relative positions, orientations, and distances among various objects. Consider FIG. 7, in which an ablation needle is shown intersecting an ultrasound image. Depending on the embodiment, it may be difficult to determine the relative angle of the ablation needle and the ultrasound image as well as the distances of various portions of the image to the ablation needle.

In some embodiments, the image guidance system may indicate spatial relationships with graphical indicators. For example, in FIGS. 8 and 9, graphical indicators help indicate the spatial relationship between a needle and an ultrasound image. These also provide an indication of the relative angle of the needle and the image.

In some unpictured embodiments, the image guidance system may draw "guidance graphics" in the form of projective lines between the needle and the ultrasound slice. These lines may be perpendicular to the plane of the slice and serve to indicate the most likely location in the slice where the needle will become visible if it is moved to become coplanar with the slice. Together with stereoscopic head-tracked visualization, the projective lines help a physician determine a more accurate assessment of the location of the needle with respect to the ultrasound slice.

Returning to FIGS. 8 and 9, in some embodiments, uniform-thickness lines between virtual needle and slice plane may be displayed on display **820** and **920**. The lines may represent the spatial relationship with three-dimensional rectangular (or any shape) needle projection bars. In various embodiments, the projection bars may be drawn perpendicular to the image, and in such a way that their small edges are aligned with (or parallel to) either the vertical (FIG. 8) or the horizontal (FIG. 9) margins of the ultrasound slice. In some embodiments, the screen-space size of the projection bars may be variable (e.g., distance-dependent) due to perspective. Thus they may provide depth cues for the physician. Further, the staircase appearance of the bars' end edges at the plane of the slice may be a further visual cue for the orientation of the needle with respect to the slice.

In some embodiments, when the needle is nearly perpendicular to the ultrasound image, the projection bars may appear similar to the needle itself. Therefore, in some embodiments, the rectangular projection bars may not be displayed when the needle is nearly perpendicular to the ultrasound image plane. Instead no projection information may be displayed or project lines may be displayed as dotted or dashed lines. The display of projection lines is illustrated in FIG. 10. In some embodiments, as depicted in FIG. 10, a line may also be drawn that is a projection of the needle onto the image plane of the ultrasound image. This may provide relative orientation information to the user or physician.

Reducing Stereo Display Artifacts with Object Choice

Stereoscopic displays separate the imagery shown to the user's eyes in various ways. Cathode Ray Tube (CRT) based devices, may use temporal sequencing, showing imagery for the left and right eye in temporal sequential alternation. This method may also be used by newer, projection-based devices, as well as by 120-Hz-switchable liquid crystal display (LCD) devices. Another type of stereoscopic display uses spatial separation such as alternating rows (AR) or alternating columns (AC). Example AR displays include the Miracube G240S, as well as Zalman Trimon Monitors. AC displays include devices manufactured by Sharp, as well as many "auto-stereoscopic" displays (e.g., Philips).

Both AR and AC monitors have reduced (often by at least 50%) resolution in one dimension: vertical for AR and horizontal for AC. As a result, some elements—most of all thin lines—when displayed as nearly horizontal AR units and nearly vertical on AC units often feature noticeable artifacts such as aliasing and discontinuities (e.g., a continuous near-horizontal line may appear dashed on an AR display). These artifacts may have a negative impact on stereoscopic fusion (e.g., the human brain's ability to merge the separate left and right eye images into a single 3D mental representation).

Stereoscopic fusion may be useful for improved perception and needle guidance by a physician. In some embodiments, an image guidance system, such as system 300 in FIG. 3A or FIG. 3B, may use thicker lines, particularly in the horizontal, and use fewer near-horizontal lines, borders, and structures when using AR displays. In some embodiments, when using an AC display, the image guidance system may use thicker lines, particularly in the vertical, and fewer near-vertical lines and structures.

In some embodiments, the projection markings such as rectangular bars shown in FIGS. 8 and 9 are chosen in part based on the type of display being used. Representing the projections in thicker form, such as rectangular bars may help overcome the limitations of AR and AC displays. Further, in some embodiments, the projection bars can be oriented along their long axes (e.g., axes that are perpendicular to the slice) such that in the case of an AR display their short end edges are aligned with the vertical edge of the ultrasound slice and thus will appear mostly vertical in the stereoscopic image. This is illustrated in FIG. 8. For AC displays, in some embodiments, the bars are oriented such that their ends are parallel to the top and bottom of the ultrasound slice and thus are more likely to appear near-horizontal in the stereoscopic image. This is depicted in FIG. 9. The projective bars were used here as an example, but this technique can be applied to any display element in order to accommodate AR or AC displays. For example, if needle drive projections are displayed in an embodiment, such as that depicted in FIG. 6, then the shape chosen to indicate the projected needle drive may be adapted (by showing spheres instead of circles, e.g., or by expanding the width of the drive indicators) to take into account that an AR or AC display is being used.

Reducing Stereo Display Ghosting Effects

In some embodiments, stereoscopic displays may suffer a "ghosting" phenomenon, which may be crosstalk between the left and right eye images. Ghosting can affect frame-sequential, AR, or AC displays. Ghosting may be exacerbated when there is a great difference between the colors or brightnesses between the left and right eye imagery shown in a region of the displayed image. Due to the nature of stereoscopic image display, these differences may occur where the (virtual) stereoscopic depth of the 3D scene to be rendered varies from the plane of the display surface.

In some embodiments, the image guidance system modifies the color and brightness of display elements that are in front of or behind the plane of the display (e.g., where the needle and ultrasound image intersect or the plane of the monitor). The image guidance system may shift the rendered color towards a uniform or background color with increasing distance from the display plane. In some embodiments, this may be accomplished by means of the OpenGL "fog" feature, which can "bathe" all displayed geometry in a color whose opacity increases with distance from the display plane. This may vary on a per-pixel basis. The farther the object is behind the display plane, the more it may be blended with the background color. This may also be applied to objects in front of the display plane by reversing the depth or Z coordinates. In some embodiments, ghosting reduction may also be implemented as a fragment shader or other routine or program, running on programmable graphics hardware or a CPU, etc. The input to a fragment program may be the color of the pixel, the color of surrounding pixels and the depth (e.g., Z depth, or the absolute distance to the plane of the monitor). The program may use the first two inputs to compute the contrast in the region local to the current pixel. The program may then reduce the contrast for those high-contrast regions, based on how far they are from the monitor's display plane. This program may also be implemented as the converse or opposite of an edge enhancement filter while also taking into account the screen depth of the edges.

Representing Non-Intersecting Objects or Images

When data related to two devices or surgical instruments are displayed with relative emplacement, it can be difficult to orient their relative locations if they do not intersect. In some embodiments, an image guidance system will render relative location information. The relative location information may be shown with color (e.g., objects may be rendered in brighter colors if they are closer), with rendering techniques (e.g., objects may be rendered with transparency so that one object behind another may be visible, but visually appear behind the closer object), with geometry (e.g., a geometric connector may be shown that will allow the viewer to discern the relative relationships), or with any other appropriate technique. FIGS. 11 and 12 illustrate example geometry and transparency being used to show relative locations of two objects.

For example, in some embodiments, if the intersection point of an ablation needle is outside of the area of the ultrasound slice, the image guidance system can draw geometry, such as a line (or rectangle) in the plane of the slice to indicate the needle's and ultrasound image's relative positions. This is depicted in FIG. 11. In some embodiments, the relative locations could also be represented using vertical and horizontal elements coplanar with the ultrasound or other image slice, as depicted in FIG. 12. In some embodiments, using geometry that is coplanar with the ultrasound image slice may provide an intuitive understanding of the relative locations of an image slice and an ablation needle.

Rendering Techniques for 3D Fusion

In some embodiments, various data displayed by the image guidance unit may be displayed as lines, frames, or 2D objects. For example, the ablation volume of FIG. 5 may be rendered as a wire-frame using 2D lines. Similarly, the projection lines of FIG. 8 may be rendered as 2D lines.

In some embodiments, some or all of the displayed data may be represented in 3D space and rendered as such. For example, the ablation volume of FIG. 5 may be represented using beam-shaped, pipe-like, swept rectangular, 3D polygonal primitives, etc. in order to "build" the wireframe representation. Similarly, the rectangular projection lines of FIG. 8 may optionally be built with beam-shaped, pipe-like, swept

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rectangular, polygonal solids, etc. For example, the projection lines of FIG. 8 may be flat rectangular prisms, and the ablation volume of FIG. 5 may be represented as thin, curved tubes with a colored stripe pattern. In some embodiments, using 3D objects to represent various data may provide improved 3D fusion for viewers.

Additionally, in some embodiments, a "surface detail" texture may be added to various objects. Adding surface detail may aid with stereo fusion because of the addition of surface texture that may provide stereoscopically "fusible" details (e.g., anchor points) on an object. A simple line or uncolored 2D object may not provide as many anchor points. Examples of possible textures include the use of color stripes or mosaics, metallic textures, and random noise textures. In some embodiments, textures may be selected so that the spatial pattern and frequency does not cause aliasing in the stereoscopic display's alternating scanlines or columns, nor with the checkerboard-interleaved pixels which are used by certain projection-based stereoscopic displays.

In some embodiments, surface shading from one or more light sources is used. Examples of surface shading that may be used includes surface shading from one or more light sources, which may be supported in graphics processor hardware, as well as other enhancements like cast shadows, and cues such as global illumination. Surface shading may contribute to increased depth perception in the guidance image.

Marking Points of Interest

In certain procedures, physicians need to keep track of multiple spots within the volume of the patient or keep track of a single point or feature while looking at other parts of the volume. For example, when a physician is going to perform an ablation, before inserting any needles, the physician will often scan the tissues at the procedures site to find all targets (e.g., tumors) and note other features of the tissues. Then, later in the procedure, the physician may return to the previously identified points-of-interest. For example, a physician might first scan the liver and find seven lesions that she will attempt to ablate. After ablating the first lesion, she must then find the second lesion again, and so forth. Before finishing the procedure, she must verify that she has ablated all seven of the lesions that she identified at the beginning of the procedure. This constant scanning and rescanning can be time consuming and error prone. Further, when if a procedure where the surgeon is attempting to locate, for example, fluid-filled cysts, once a needle pierces the cyst, the fluid may drain out, making the target difficult or impossible to locate again with ultrasound.

In some embodiments, the image guidance system may allow the physician to mark or keep track of points or features of interest. In various embodiments, the physician can mark the points or features of interest in various ways. For example, consider a procedure where the doctor is using the image guidance system with an ablation needle and an ultrasound wand. The doctor may be able to mark the point by pressing a button on a keyboard or medical device, by gesturing or issuing a verbal command, or with any other appropriate method. The point of interest may be marked at the point where the needle intersects with the ultrasound image plane, where the needle's projection intersects with the ultrasound image plane, or any other appropriate relationship (such as at the location of the tip of the needle). For example, when the physician identifies a point-of-interest **1301** within the ultrasound image, she can point to it using the needle even if the needle is outside the body of the patient. This is depicted in FIG. 13. The physician (or assistant) may then press, for example, a button or foot pedal, which informs the image guidance system to store the 3D position of this point-of-

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interest **1301**. FIG. 14 illustrates an X being displayed where a point of interest **1401** has been marked. In some embodiments, the system may then display the position of this point-of-interest **1401** relative to the ultrasound plane and the needle. For example, an X-shaped marker **1502** may be displayed on display **1520** to show the relative position of the marked position and the surgical instruments, as depicted in FIG. 15. In some embodiments, the system may also display a bar that connects the X marker **1502** of the point-of-interest to the nearest point (or the point to which a normal vector of the image plane would reach the X), as depicted in FIG. 15. This visually indicates, to the physician, the distance between the ultrasound image and this point-of-interest. Should the physician want to see the point of interest again in the live ultrasound image, the graphics indicate to where she should move the ultrasound transducer to view that point in the ultrasound image. In some embodiments, the image guidance system may also display the numerical distance (e.g., in mm) between the ultrasound image and the point-of-interest (not shown).

Physicians, during some liver ablation procedures, may manage fifteen points-of-interest, or even more. As depicted in FIG. 15, in some embodiments, there may also be multiple markers **1502** of point of interest simultaneously displayed. The image guidance system may be able to store and display any number of points of interest simultaneously. If there is more than one point-of-interest in view, the image guidance system may display a number next to each one (not pictured). In some embodiments, in order to reduce visual clutter if there are many points of interest, those points which are closer to the ultrasound image plane are drawn more saliently or vividly (with more bold color and thicker lines) while the points that are far away are drawn less saliently (more transparent, blurred, muted colors, etc.). Additionally, in various embodiments, other representations other than an X (such as a point, point cloud, sphere, box, etc.) may be used and multiple markers or locations may be represented with different markings.

In some embodiments, the image guidance system stores the points-of-interests' positions in the position sensing system's coordinate system. If the position sensing system is fixed to the image guidance system, then, if the patient or image guidance system are moved, stored points-of-interest may become incorrectly located. In some embodiments, this can be remedied via a fiducial or other detectable feature or item, the pose of which relative to the tracking system may be continually, continuously, periodically, or occasionally measured. The fiducial may be attached to the operating table, the patient's skin, or even embedded into the tissue itself (e.g., as a magnetic tracking coil), and the points-of-interest' positions, relative to it, can be stored and displayed. For example, in a system where magnetic tracking is used, a magnetic tracking coil may be affixed to the operating table or patient.

Data Visualization Processes and Data

Displaying Volumetric Data

There are numerous types of volumetric or 3D data that various embodiments of the image guidance system herein may display. Such data may include CT scans, MRI, PET, 3D ultrasound, and any of numerous other types of 3D data. In some embodiments, in order to display 3D data on a 2D interface, such as a computer screen, or even a 3D interface, such as a head-mounted display or other 3D display, a subset of the data is chosen to display. This subset of data can include axis-aligned slices, the entire volume, or a sub-volume of the data. An inherent difficulty with image guidance is the display of three dimensions of data on a two dimensional screen or "dual eye" three dimensional display. When displaying 3D

data, such as CT scans, a system might only display a single plane, or show three orthogonal planes separately on the screen, as shown in FIG. 1. The data may also be shown as a volumetric 'block' of data, as shown in FIG. 2.

Therefore, as depicted in FIG. 2, if a sub-volume is displayed, the outer surface of the volume may be displayed as a box on the screen and the data interior to the rendered box may not be visible to the doctor. The 3D data may be displayed in correspondence to the surgical instrument that the doctor is holding (e.g., note the needle and 3D data interacting in FIG. 2). The 3D data may also be displayed as axis-aligned slices, as shown in FIG. 1. In previous systems, when the doctor wanted a different view of the 3D data (either a different volume, as in FIG. 2, or different set of images, as in FIG. 1), she would have to alter the location of the displayed planes, using, for example, a cursor (controlled by a mouse or trackball).

In some embodiments, the image guidance system controls the display of the 3D data with a medical device. For example, as depicted in FIG. 16, one of the planes 1603 of the 3D data displayed on display 1620 may be aligned with a tracked surgical needle, such as surgical needle 1645. Additionally, in some embodiments, separate data related to another medical device, such as ultrasound data, may be displayed on display 1620 (not shown). This data may be obtained, and its pose or emplacement known, based on a tracked ultrasound wand, such as tracked ultrasound wand 1655 of FIG. 16.

In some embodiments, the displayed plane 1603 of the 3D data may be axis-aligned in one direction and controlled by the surgical instrument in the other two directions. This may result in an image such as that displayed in FIG. 16, where the image is aligned with the, or Y axis, and the location in the X and Y axes is controlled by the needle placement. The plane of orientation of the surface may also be chosen based on alignment with the plane of the display (choose the closest plane to the screen's plane); closest to one of the three traditional orthogonal planes (sagittal, transverse, coronal); or one specified by the physician (or an assistant who is not in the sterile field), using a control knob, lever, or foot pedal. If the needle is curved (or bent into a curve from the pressures acting on it by the tissues and the physician's hand), the system may choose the plane that most clearly displays the curvature of the needle.

In some embodiments, the display plane may also be controlled by the rotation of the medical device. This is depicted in FIG. 17, which illustrates that, once the needle 1745 is rotated, the display plane for the volumetric data is rotated and shown in display 1720. In some embodiments, the image guidance system may choose a plane that intersects some feature or landmark on the needle's handle (such as the port where the wire exits, or a molded ridge) or the needle's shaft (such as the openings in the shaft from which the paddles deploy on the needles made by RFA Medical™). Then, when the physician physically twists the needle, it has the effect of rotating the cross-sectional plane (FIG. 4). This may allow a physician to intuitively specify its orientation by using the needle. The rotational arrows in FIG. 17, in various embodiments, may or may not be shown on display 1720.

The system can work with static or real-time (or near real-time) volumetric data. In some embodiments, the system may display a cross section of the volumetric image along a plane that intersects the axis of a surgical needle or other surgical or medical device. The system may continually update the position and orientation of the cross-sectional plane as the physician moves the needle. If the volumetric or 3D image data is from a real-time imager, such as a 3D ultrasound transducer, then instead of having to continually

manipulate both the needle and transducer, the physician may place the transducer such that the ultrasound volume includes the target, and then to leave the transducer stationary. She then can manipulate the needle's position, before it pierces the tissues, until the target tissue appears visible in the slice controlled by the needle.

Physicians often attempt to maintain 2D ultrasound planes in order to keep the shaft of the needle within the ultrasound image. Doing so may allow then to watch as the needle advances through the tissues. In some embodiments herein, the image guidance system may maintain the displayed ultrasound image within the needle's path automatically. If the doctor can see what is in the needle's path (as shown in the displayed plane of the 3D volumetric data) she may be able to see what will be in the needle's path when she drives the needle. By being able to see this, she may be able to avoid piercing any tissue that should not be pierced by the needle's path. In some embodiments, as the physician advances the needle towards a target, the cross-sectional plane may be chosen automatically by the image guidance system such that it shows the needle, the tissue surrounding the needle, and any structures that are about to be pierced by the needle.

In some embodiments, similar techniques can be used to control the images that are displayed in 2D, as in FIG. 1. That is, the manipulation of a medical device, such as a needle, scalpel, ultrasound wand, etc. can control what planes are shown in the display. For example, if a surgeon moved a needle toward and away from herself, she might sweep through the 3D volume and the corresponding slices of the 3D volume may be shown on the display.

As noted above, various embodiments use live or real-time volumetric images (e.g., intraoperative 3D ultrasound), static volumetric images (e.g., pre-operative CT or MRI) or hybrid volumetric images (e.g., pre-operative CT images that are continuously warped to be in registration with live 2D ultrasound or fluoroscopic images, or laser-scanned 3D point sets representing the surface of tissue).

Visualizing Portions of Volumetric Data

When displaying 3D volumetric data, voxels in front (closer to the virtual camera) typically obscure the voxels behind them. This hides information that may be important from preoperative 3D data and real-time or live 3D data because the surgeon can only clearly view the closest voxels. As noted above, one way to deal with displaying volumetric data is to allow the doctor to view the data as 2D slices, in cross section, etc. In some instances, however, there are determinable differences among the voxels in the 3D data. Therefore, in some embodiments, the image guidance system can display only those voxels that meet certain criteria. For example, in the case of a preoperative CT scan, the voxels containing bone matter should be determinable based on tissue density. Therefore, the image guidance system may display only those voxels within a certain range of tissue densities. As another example, when the volumetric image of a fetus in the womb is visualized from 3D ultrasound data, embodiments of the image guidance system may make all voxels that represent fluid surrounding the fetus transparent or invisible, thus allowing the surface of the fetus to be visible.

Some types of 3D imaging data can provide flow information. In some embodiments, the image guidance system can be set to only display only those voxels that contain flow information. For example, some ultrasound scanners, including 3D ultrasound scanners, can measure motion and flow within the imaged area using Doppler techniques. The portions of the image that have flow above some threshold velocity may be displayed using a particular color or a gradient of

colors determined based on the flow information. The remainder, non-flowing part of the ultrasound image may be drawn as traditional grayscale, or may be made invisible.

For example, in some embodiments, the image guidance system may have a Doppler 3D mode, in which volumetric images (such as a 3D ultrasound) are sampled, and then those volumetric images are displayed such that only those voxels which contain flow (above some threshold velocity) are opaque, while all other voxels (without sufficient flow) are made transparent. By displaying only the portions of the image that have Doppler-detected motion, the image guidance system may provide an easy-to-decipher 3D image of the progress of the ablation. For example, FIG. 18 illustrates a needle 1845 ablating tissue while a 3D ultrasound wand 1855 is collecting ultrasound data. The Doppler data is collected from 3D ultrasound wand 1855 and only the progress of the ablation 1804 is shown on display 1820. One or more slices of the collected ultrasound data may also be shown on display 1820 (not pictured).

In some embodiments, Doppler information can be collected over time as the doctor sweeps a 2D ultrasound wand over a volume. Since the ultrasound wand is tracked, the image guidance system can determine the relative locations of the collected ultrasound slices and locate them in 3D space. From this data, in some embodiments, the image guidance data can approximate 3D flow information in various ways. For example, in some embodiments, in order to observe the progression of the ablation with a 2D transducer, the physician may continually sweep the ultrasound transducer back and forth over the general area of tissue that contains the lesion and ablation needle. Some of the tissue being ablated contains may expand into micro bubbles that can be detected in ultrasound. The image guidance system may extract those pixels and represent the area of Doppler flow (e.g., "a Doppler slice"), relative to the latest 2D ultrasound image ("the ultrasound slice"). For example, as depicted in FIG. 19, as 2D ultrasound wand 1955 is swept across the volume of interest, Doppler slices 1921 may be collected and displayed on display 1920. Additionally, the ultrasound slice 1922 may also be displayed. Optionally, ultrasound needle 1945 may also be displayed on display 1920.

In some embodiments, older Doppler slices may be drawn more transparently, with more blur, in order to reflect that, the older a slice is, the more out-of-date its image contents have become. Eventually, every sampled slice may become completely invisible, no longer being presented to the user. This prevents out-of-date images from obscuring the view of more recent images.

In some embodiments, the ultrasound slices are rendered using various techniques. For example, they might be rendered using a technique from Garrett et al., *Real-Time Incremental Visualization of Dynamic Ultrasound Volumes Using Parallel BSP Trees*. Proc. IEEE Visualization '96 (San Francisco, Calif., Oct. 27-Nov. 1, 1996), pp. 235-240, 490, which is hereby incorporated by reference for all purposes. For example, each rendering frame, a binary spatial partition (BSP) tree data structure may be used to compute a back-to-front ordering of each slice. Then the slices may then be rendered in back-to-front order, such that the transparency and occlusion are handled correctly. Reconstruct, in 3D, only the portions of the image that have Doppler-detected motion may make the 3D images easier for the physician to decipher, thereby improving her understanding of the progression of the ablation.

In some embodiments, a rendering technique is used to sort Doppler slices using the depth of the center-point of each Doppler slice. This technique may result in an approximate

back-to-front ordering as the slices may intersect. In some embodiments, a BSP tree algorithm may split one slice into two in the case where they intersect each other. Since sorting by the slices' center point depths results in an approximate ordering, the resulting rendering may have some visual artifacts (e.g., pieces of one slice that should appear to be behind another slice, but instead appear in front of it). To minimize the presence of these artifacts, in some embodiments, the image guidance system may render the Doppler slices in two separate passes. In the first pass, a clipping plane, co-incident with the most recent ultrasound slice, is employed to discard the portions of any Doppler slices that are in front of the ultrasound slice. Then the ultrasound slice is drawn, followed by the second pass of the Doppler slices. This second time, the clipping plane discards the portions of any Doppler slices that lie behind the ultrasound slice.

Thin Visualization of 3D Data

As noted above, in traditional rendering of 3D volumetric data, data or voxels in the front of the rendered image may occlude data or voxels towards the back of the volume. This may be a problem when the data that is further back from the surface is the information that a physician needs to see. Various techniques for overcoming this are given above. More techniques are given in this section.

In some embodiments, the 3D volume data herein may be rendered with a "thin" field of view or depth of focus. For example, in some embodiments, the image guidance system renders a single plane-of-interest in sharp focus, while rendering the rest of the volume dataset, in perspective projection, as transparent and blurry, with stereo cues and/or motion parallax, and spatially registered to the plane-of-interest. This provides the user some context and representation for features located outside of the plane-of-interest, while minimizing their visual interference with image features in the plane-of-interest. In some embodiments, a thin volume of interest (as opposed to a plane of interest) may also be rendered. The volume of interest may include a small and/or user-controllable slice of data that is rendered in sharp focus with, as above, the rest of the volumetric data (in front of and behind) the thin volume of interest rendered in a blurry, transparent, or other technique.

This thin depth-of-field volume visualization may have several medical applications. It may be useful to help the physician/user guide a needle towards a target located in the plane-of-interest, while simultaneously avoiding features in front of or behind the plane-of-interest. It may also be used to identify and mark features (e.g., points, organ boundaries, tumors) in the volumetric images (described above). These tasks can be performed with real-time volumetric images (e.g., intraoperative 3D ultrasound), static volumetric images (pre-operative CT, MRI, etc.) or hybrid volumetric images (e.g., pre-operative CT images that are continuously warped to be in registration with live 2D ultrasound or fluoroscopic images, or laser-scanned 3D point sets representing the surface of tissue).

Further, this technique can be combined with other techniques herein. For example, in order to control the plane or volume of interest (location, orientation), a surgeon may manipulate the needle as described above. In some embodiments, the plane or volume of interest may be parallel and coincident with the screen-plane1, or it may have some other spatial relationship to the surface of the display screen. For example, the plane or volume of interest may contain the needle that the physician is placing into the tissue. In some embodiments, the doctor or other user may interactively manipulate the spatial relationship of the plane or volume of

interest relative to the volume dataset, using the needle, or by controlling a knob, mouse, joystick, etc.

In some embodiments, the thin depth-of-field volume can be displayed such that it is superimposed and spatially registered with organ/blood vessel/tumor surfaces or contours, radiation dose iso-contours, needle guidance information, or any other combination of relevant known polygonal or volumetric 3D data.

In some embodiments, when used with stereoscopic monitors, thin depth-of-field rendering can also be used to reduce ghosting (an undesired cross-talk between the two separate images for each eye. For example, a high-contrast line in the left-eye image may be slightly visible in the right-eye image). When used to reduce ghosting, the volume or plane of interest may be co-incident or nearly co-incident with the screen plane in 3D space (e.g., the surface of the display monitor).

In some embodiments, the volumetric data is sliced (e.g., resampled) into a set of image planes or image volumes that are parallel to the plane of interest. The distance between the image planes or volumes may be dependent on the resolution of the volume dataset, the display monitor's resolution, and the computational resources available (e.g., larger spacing may result in faster rendering and a higher frame rate, but a lower fidelity image in each frame). For example, an image plane (or volume) may be created for each depth resolution in the volumetric data, or a predefined or determined number of slices may be used. Each image plane or volume is then blurred; the "radius" of the blur may increase with the distance from the image slice to the plane or volume of interest (e.g., images slices further from the plane of interest may be made blurrier than image slices close to the plane-of-interest). The image plane coincident with the plane-of-interest itself may have no blur (e.g., it may be rendered using the standard reconstruction for the display monitor's resolution). In some embodiments, the image planes' brightness, contrast and/or transparency may then be modulated by their distance from the plane or volume of interest. In some embodiments, the planes may then be rendered in back-to-front order. Various embodiments may also be implemented directly on programmable graphics hardware, dedicated hardware, etc. to reduce processing time and or memory usage.

In some embodiments, in order to reduce computational and memory demands, the image planes may be spaced such that the further they are from the plane-of-interest, the larger the distance between them. Those portions of the volume dataset that are farther away from the plane-of-interest, and thus displayed as blurrier and more transparent, will have a lower density of image-planes that sample them.

Tracking and Calibration

Image guidance systems provide real-time guidance to a medical practitioner during medical procedures. Numerous examples and embodiments of this are given herein. Image guidance systems require tracking. In order to track, there is typically a tracking "source" and a tracking "receiver," although there are many other arrangements known to those skilled in the art and discussed herein. Examples of tracking are discussed throughout herein and with respect to instruments 345 and 355 and tracking systems 310 and 340 in FIGS. 3A and 3B.

In order to track a device, some portion of the tracking system must be attached to the device. In some instances this may actually be a source, receiver, fiducial, etc. In optical tracking, for example, a tracking device is employed by the system to continually report the position and/or orientation of tracking fiducials that are attached to the devices to be tracked. In some embodiments, these fiducials are rigidly affixed to the needle or to its handle. With knowledge of the

geometry of the needle, relative to the fiducials, an image guidance system can compute the position of the needle and its tip.

As noted above, each time a medical practitioner uses a new needle with a guidance system, she must rigidly affix the tracking fiducials to the needle and she must measure the position of the tip of the needle, relative to the fiducials. This is an extremely time consuming process. She must first tighten screws, or to thread the needle through a hole or tube. Then she must manually measure the needle length with a ruler (because needle lengths may vary even for standard needles), and then enter this information into a workstation. She may also be able to use a dedicated calibration rig, and perform a lengthy, often minutes-long calibration process. The same process occurs for other types of tracking systems as well.

Simplifying Calibration

In order to simplify the calibration process, in some embodiments, the image guidance systems can utilize something that will indicate the needle's tip relative to a known or determinable location. If the needle is being tracked (even if not calibrated) when this is done, then the needle's tip relative to its own tracking fiducials can be calculated. For example, consider a needle's fiducial mount 2000 comprising a spring-loaded plastic clip 2010, with a groove embedded in the inner surfaces of both of the inner sides of the clip. In some embodiments, the tracking fiducials 2040 may be attached to a fixed piece of the clamp. The user may attach the needle by first pressing onto the side opposite the fulcrum to open the "jaws" (as depicted in FIG. 20). She may then insert the needle 2020 into the groove on the fixed part of the clamp while maintaining pressure upon the upper sides, above the pivot point, of the jaw with her thumb; she can then release her thumb. In some embodiments, she may perform this maneuver such that the distal end of the needle's shaft 2030 is flush with one end of the clip 2010. The spring may force the jaws 2010 to grip the needle shaft 2030, rather than being secured by a screw. In some embodiments, this design accommodates needles of varying shaft diameters. Also, in various embodiments, the needle 2020 is inserted by moving in a direction roughly perpendicular to its shaft axis and this may create a situation in which the tip of the needle does not come close to the jaws. This may reduce the chance of damage to the needle tip from the jaws, and further, allow mount to be removed even if the needle is still embedded in tissues.

In some embodiments, the spring action may be from a metal or other ancillary spring between the plastic. In some embodiments, the spring may be a coil or bent wedge design. In some embodiments, an integrated plastic or native material spring may also be incorporated into the molded parts. In some embodiments, the clamp components may be both molded, machined, or a combination thereof. In some embodiments, the materials may be medical grade plastic, which may provide light weight. The material may also be stainless steel, which may provide for easier or more economically sterilization. The apparatus can be made of any combination of plastic, metal, and ceramic, and can be fabricated by machining, casting, molding, or rapid prototyping (SLA, SLS, FDM, EBM, etc.). Further, in various embodiments, the needle may vibrate or heat up and the design of the needle mount's jaw accommodates this.

A second tracked device, rig, or mount 2100 of FIG. 21 may provide the frame or reference. This tracked device 2100 may be something that is dedicated for this purpose, or it may be a tracked surgical device 2100 that is appropriately configured. For example, an ultrasound transducer may also be tracked. In some embodiments, the ultrasound transducer's

tracking (fiducial) mount has divot, groove, etc. **2110** in it for receiving the needle tip. This is depicted in FIG. **21**. The location of the divot relative to the ultrasound transducer's fiducials is known. Therefore, in some embodiments, by touching the needle tip to this divot as depicted in FIG. **22** at position **2201**, the system can compute the needle tip's position relative to the fiducials attached to the needle.

Example embodiments of performing this calculation are as follows:

The rigid body transformations listed below (which can be represented by 4x4 matrices, quaternions, etc.) may be known by the image guidance system:

transducerFiducials_from_tracker (the position and orientation of the ultrasound transducer's fiducials, relative to the tracking device's reference coordinate system)

needleFiducials_from_tracker (the position and orientation of the needle's fiducials, relative to the tracking device's reference coordinate system)

This position is also known: (which can be presented by a 4-element vector: {x,y,z,1}) divot_in_transducerFiducials (the position of the divot relative to the ultrasound transducer's fiducials)

In order to find needleTip_in_needleFiducials (the relative locations or transformation between the needle tip and the fiducials attached to the needles), various embodiments may perform the following calculations when the needle tip touches the divot:

needleTip_in_needleFiducials=divot_in_needleFiducials

needleTip_in_needleFiducials=divot_in_tracker*

tracker_from_needleFiducials

needleTip_in_needleFiducials=divot_in_transducerFiducials*transducerFiducials_from_tracker*((needleFiducials_from_tracker)-1)

In some embodiments, the user may perform some or all of the following actions before the calculations above are performed:

- 1) The user may hold a needle tip in the divot and simultaneously presses a foot pedal to record their positions. As an alternative to a foot pedal, the user might ask her assistant to press a button (because the user herself cannot press the button as she has both hands occupied).
- 2) The user may hold down a foot pedal and hold the needle in the divot, then moves the transducer and needle together for roughly one second, while maintaining the needle in the divot, and then releases the foot pedal. This may result in more samples of positions and relative positions and may allow the system to more accurately determine (via regression, averaging, or other calculations) the position of the tip of the needle, relative to the needle fiducials.

Additionally, the image guidance system may be able to detect when the needle is in the divot by a gesture, voice command, duration in a single position, or any other appropriate method.

Various embodiments of these techniques may be used by any kind of medical professional—veterinarian, physician, surgeon, emergency medical technician, physician's assistant, nurse, etc. Various embodiments use different kinds of rigid needles, needle-like devices (e.g. radiofrequency or microwave ablation probe, cryo-ablation probe, cannula, optical waveguide, harmonic dissector, etc.). Various embodiments provide for the relative locations of a scalpel (where the divot may be replaced by a notched groove in order to locate the position of the scalpel, its tip, etc.).

Various embodiments of tracking the various devices, such as devices **2100** and **2000**, are discussed throughout herein and with respect to position sensing units **310** and **340** of FIGS. **3A** and **3B**. If optical tracking is used and the tracking

system measures only the position of each fiducial, then three or more such fiducials may be affixed to the needle in order to compute the orientation of the needle. Otherwise, fewer than three fiducials may be attached.

5 Rendering Techniques

Asynchronous Rendering

As noted above, real-time, live, or intraoperative data may be used and rendered in various embodiments herein. The update rate of the various data used may differ, and some may be slow enough, that if the entire image were only updated at that rate, a physician may be able to notice the update, which may be undesirable. For example, if an ultrasound were only updated once per second and the entire scene were only rendered once per second, the physician is likely to notice this and find the system unusable. Perceivable lag can increase the risk of simulator sickness, and the system might appear unresponsive. In various embodiments, the 3D display herein is designed to reduce response time and may appear to match the physician's movements with less or no perceivable lag. To accomplish this, various embodiments use asynchronous rendering. In some embodiments, no process or operation in a thread that renders the video or screen images waits for new data from the data from the other devices or systems, such as the tracking system or ultrasound scanner. Instead those threads use the latest available data. In some embodiments, two accessory threads query the tracker (such as position sensing units **310** and **340** in FIGS. **3A** and **3B**) and a video frame grabber, which may be part of an image guidance system such as image guidance system **300** of FIGS. **3A** and **3B**. These threads wait as their respective hardware delivers the requested data, and then update the main thread's relevant data structures as soon as they have new data, without causing the main thread to wait. Therefore, the main or graphical rendering thread can continue to update the image with whatever data is available for the tracking, imaging, and other data.

Similarly, the image guidance unit's main thread may instruct associated graphics hardware to swap the front and back display buffers immediately after drawing a new image in the back buffer, without waiting for the vertical sync signal. This allows the newly drawn graphics to appear on the display monitor sooner, and may allow for a higher graphics frame rate. Using this asynchronous technique a user might notice tearing in both the ultrasound image and in the graphics display. However, in some embodiments, the image guidance system grabs video frames much faster than an imager, such as an ultrasound scanner generates frames. The image guidance system may also draw frames much faster than the refresh rate of the LCD display monitor. As such, any tearing between successive frames will be evenly distributed, and may be less noticeable to the human eye. At a 60 Hz video refresh rate, we would expect that 17 ms ($\frac{1}{60}$ Hz) of latency may be avoided by not waiting for vertical sync. In some embodiments, latency may be reduced by up to 70 ms (or more).

These techniques may allow for low latency without requiring the various sub-systems to necessarily be tuned to each other or wait for each other.

Other Exemplary Embodiments for Various Procedures

Removal of Fibroids

In some embodiments, the image guidance system may be used to remove fibroids, while leaving the uterine muscle wall strong enough to carry a fetus. For example, when a physician finds a fibroid with a tracked laparoscopic ultrasound, the image guidance system, such as system **300** of FIGS. **3A** and **3B**, may display a visualization of a dissection tool relative to the fibroid in the ultrasound image. This may help the physician cut the muscle wall down the midline of the fibroid, or

other desired cut approach. Such embodiments may reduce the damage the muscle wall, which may then be more likely to support pregnancy. These embodiments may also reduce the amount of stitching, and reduce the time to remove a fibroid.

In some embodiments, the system may be configured to allow for ablation of fibroids. For example, system **300** of FIGS. **3A** and **3B** may include a tracked ablation antenna **345** and a tracked external ultrasound probe **355**, laparoscopic ultrasound transducer **355**, etc. The image guidance unit **330** may provide guidance information on the display **320**, e.g., including the relative positions or emplacements of the fibroid in the ultrasound image and the tip, projection, and/or expected ablation volume of the ablation needle **345**. This guidance information may allow the physician to more quickly locate and place the ablation needle into fibroids.

Today, surgeons often target fibroids 3-4 cm wide. In some embodiments, a surgeon may be able to find smaller fibroids (such as those 1 cm wide and smaller) because of the accuracy of the tracking and imaging, thereby increasing the probability of the patient carrying a baby to term, and decreasing other symptoms resulting from fibroids.

Ablation of Pancreatic Cysts

Pancreatic cysts may be a precursor to pancreatic cancer. Therefore, it may be useful to ablate the pancreatic cysts when they occur, whether or not it is certain that pancreatic cancer would necessarily follow.

In some embodiments, the image guidance system may be used aid a physician in ablating the pancreatic cysts. For example, in some embodiments, an image guidance system, such as the system **300** of FIGS. **3A** and **3B** may include an endoscopic ultrasound transducer **355** and an ablator **345**, such as an ablation needle **345**. In some embodiments, the ablator uses laser light, microwave, radio wave, or any other appropriate ablation energy or technique. In some embodiments, the ultrasound transducer is inserted via the mouth and images the pancreas through the wall of stomach or duodenum, while the ablation needle enters the patient from outside the body.

Hysteroscopy

Some physicians remove fibroids using a hysteroscope, or other flexible endoscope that passes through the vagina and cervix and functions inside the uterus. Hysteroscopy may be less invasive than other forms of laparoscopic surgery because of the lack of incision and insufflation. Further, hysteroscopy can sometimes be performed in a clinic instead of a hospital, thereby potentially reducing costs.

In some embodiments, a hysteroscope is tracked and imaged by an image guidance system, such as system **300** of FIGS. **3A** and **3B**. In order to image fibroids, a physician may use external ultrasound, filling the bladder with water so that she can image through it and see the uterus. In some embodiments, a resectoscope, which may be a hysteroscope with a wire loop extending from it, may be used by the physician and with an embodiment of the image guidance system. The resectoscope may have a semi-circular loop in a plane parallel to the image plane that can translate forward and back (toward and away from the lens). The wire loop may be energized (e.g., electrocauterizer) and carve away a detected fibroid. In some embodiments, the image guidance system may track the resectoscope or hysteroscope and render the resector wire loop, relative to the ultrasound scan or any other devices used.

Harvesting Eggs

In some embodiments, the image guidance system is used to track and visualize the ultrasound data as well as the needle that is used to collect the eggs from the ovary. For example, in order to harvest eggs a transvaginal ultrasound probe to visualize the follicles in the ovary, which may contain eggs, may

be used. The image guidance may help the physician get a flexible needle (16 gauge, 30 cm long) into each follicle, through the vaginal wall. A physician may push on the outside of the patient to push the ovary into a position where it can be imaged and accessed through the vaginal wall. Each follicle containing an egg is typically 1-2 cm wide. The physician may drain (aspirate) the contents of the follicle, and then examine the fluid to look for an egg. The physician may then proceed to the next follicle. She may collect 9-10 eggs, or even more. Eggs are often attached to the side of the follicle, and the needle should enter the center of the follicle in order to safely remove it from the wall. Embodiments herein make that targeting easier by tracking the needle and the ultrasound (or other imaging) that is used to find the eggs. Such embodiments used for this procedure may be a more effective procedure than is currently available.

Embryo Attachment

In some embodiments, the image guidance system is used for embryo attachment or embryo transfer. Embryos are inserted via a flexible catheter through the cervix. The catheter consists of a flexible inner tube within a more rigid external tube, each about 10-20 cm long. While the inner tube may be very flexible, the outer tube may be stiffer and allows a physician to guide the inner tube. The physician may fill the bladder with water, and uses external ultrasound to image the uterus through the bladder. The ideal place to implant the embryos is the "maximal implantation potential (MIP) point", which is roughly the "top" of the uterus, between the fallopian tubes. A surgeon may use ultrasound to find this point (possibly marking the point as discussed herein), and guide the catheter there. The goal is to implant between the two layers of the uterine lining, but "it's hard to see where the tip goes" once it is inside the uterine lining.

The catheter and/or the tip of the inner tube may be tracked and its emplacement relative to the ultrasound image may be displayed to the physician via the image guidance system. For example, the tip of the catheter may be tracked and its real-time emplacement shown relative to the ultrasound image or marked MIP. In some embodiments, in addition to tracking the very tip of the inner catheter, the image guidance system also tracks one or more points along the catheter. As such, the image guidance system can display the catheter's shape near its tip.

If a physician can get the embryo into the right place, it may increase the overall success rate. This, in turn, could eventually allow physicians to implant fewer embryos, perhaps reducing the "twin rate."

The processes, computer readable medium, and systems described herein may be performed on various types of hardware, such as computer systems. In computer systems may include a bus or other communication mechanism for communicating information, and a processor coupled with the bus for processing information. A computer system may have a main memory, such as a random access memory or other dynamic storage device, coupled to the bus. The main memory may be used to store instructions and temporary variables. The computer system may also include a read-only memory or other static storage device coupled to the bus for storing static information and instructions. The computer system may also be coupled to a display, such as a CRT or LCD monitor. Input devices may also be coupled to the computer system. These input devices may include a mouse, a trackball, or cursor direction keys. Computer systems described herein may include the image guidance unit **330**, first and second position sensing units **310** and **340**, and imaging unit **350**. Each computer system may be implemented using one or more physical computers or computer systems or portions

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thereof. The instructions executed by the computer system may also be read in from a computer-readable medium. The computer-readable medium may be a CD, DVD, optical or magnetic disk, laserdisc, carrier wave, or any other medium that is readable by the computer system. In some embodiments, hardwired circuitry may be used in place of or in combination with software instructions executed by the processor.

As will be apparent, the features and attributes of the specific embodiments disclosed above may be combined in different ways to form additional embodiments, all of which fall within the scope of the present disclosure.

Conditional language used herein, such as, among others, “can,” “could,” “might,” “may,” “e.g.,” and the like, unless specifically stated otherwise, or otherwise understood within the context as used, is generally intended to convey that certain embodiments include, while other embodiments do not include, certain features, elements and/or states. Thus, such conditional language is not generally intended to imply that features, elements and/or states are in any way required for one or more embodiments or that one or more embodiments necessarily include logic for deciding, with or without author input or prompting, whether these features, elements and/or states are included or are to be performed in any particular embodiment.

Any process descriptions, elements, or blocks in the flow diagrams described herein and/or depicted in the attached figures should be understood as potentially representing modules, segments, or portions of code which include one or more executable instructions for implementing specific logical functions or steps in the process. Alternate implementations are included within the scope of the embodiments described herein in which elements or functions may be deleted, executed out of order from that shown or discussed, including substantially concurrently or in reverse order, depending on the functionality involved, as would be understood by those skilled in the art.

All of the methods and processes described above may be embodied in, and fully automated via, software code modules executed by one or more general purpose computers or processors, such as those computer systems described above. The code modules may be stored in any type of computer-readable medium or other computer storage device. Some or all of the methods may alternatively be embodied in specialized computer hardware.

It should be emphasized that many variations and modifications may be made to the above-described embodiments, the elements of which are to be understood as being among other acceptable examples. All such modifications and variations are intended to be included herein within the scope of this disclosure and protected by the following claims.

What is claimed is:

1. A method, comprising:

determining, with one or more processors, real-time position and orientation of a first medical device;
determining, with the one or more processors, real-time position and orientation of a second medical device;
determining position and orientation of a 2D image area based at least in part on the determined real-time position and orientation of the second medical device;
receiving in real-time image data for the 2D image area from the second medical device;
determining a perspective view of the 2D image area in a virtual 3D space based at least in part on a relative orientation of the second medical device with respect to

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an expected location of a user, wherein the expected location of the user is a fixed location in front of one or more displays; and

causing the one or more displays to display in real-time a perspective view of an image corresponding to the image data in the virtual 3D space based at least in part on the determined perspective view of the 2D image area.

2. The method of claim 1, further comprising causing the one or more displays to display in real-time a perspective view of a virtual medical device corresponding to the first medical device based at least in part on the relative orientation of the first medical device with respect to the expected location of the user.

3. The method of claim 1, further comprising causing the one or more displays to display a 2D view of the image corresponding to the image data.

4. The method of claim 1, further comprising causing the one or more displays to display a graphic indicating an intersection between a trajectory of the first medical device and the 2D image area.

5. The method of claim 1, further comprising causing the one or more displays to display a graphic indicating an intersection between a trajectory of the first medical device and a location on a 2D plane corresponding to the 2D image area, wherein the location on the 2D plane is outside the 2D image area.

6. The method of claim 1, wherein the first medical device comprises an ablation needle, and wherein the method further comprises causing the one or more displays to display in real-time a perspective view of an ablation volume for the ablation needle in the virtual 3D space based at least in part on the relative orientation of the first medical device with respect to the expected location of the user.

7. The method of claim 1, further comprising:

receiving an indication of a point of interest;
marking in an underlying 3D model an intersection of a trajectory of the first medical device and a 2D plane corresponding to the 2D image area as the point of interest; and

causing the one or more displays to display in real-time a perspective view of the point of interest in the virtual 3D space based at least in part on the determined perspective view of the 2D image area.

8. The method of claim 1, wherein the first medical device comprises a needle and the second medical device comprises an imaging device.

9. A system, comprising:

a computing device comprising one or more processors, the computing device configured to:

determine real-time position and orientation of a first medical device based at least in part on data received from a first pose sensor;
determine real-time position and orientation of a second medical device based at least in part on data received from a second pose sensor;
determine position and orientation of a 2D image area based at least in part on the determined real-time position and orientation of the second medical device;
receive image data for the 2D image area from the second medical device;

determine a perspective view of the 2D image area in a virtual 3D space based at least in part on a relative orientation of the second medical device with respect to an expected location of a user, wherein the expected location of the user is a fixed location in front of one or more displays; and

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cause the one or more displays to display in real-time a perspective view of an image corresponding to the image data in the virtual 3D space based at least in part on the determined perspective view of the 2D image area.

10. The system of claim 9, wherein the computing device is further configured to cause the one or more displays to display in real-time a perspective view of a virtual medical device corresponding to the first medical device based at least in part on the relative orientation of the first medical device with respect to the expected location of the user.

11. The system of claim 9, wherein the computing device is further configured to cause the one or more displays to display a 2D view of the image corresponding to the image data.

12. The system of claim 9, wherein the computing device is further configured to cause the one or more displays to display a graphic indicating an intersection between a trajectory of the first medical device and the 2D image area.

13. The system of claim 9, wherein the computing device is further configured to cause the one or more displays to display a graphic indicating an intersection between a trajectory of the first medical device and a location on a 2D plane corresponding to the 2D image area, wherein the location on the 2D plane is outside the 2D image area.

14. The system of claim 9, wherein the first medical device comprises an ablation needle and the computing device is further configured to cause the one or more displays to display in real-time a perspective view of an ablation volume for the ablation needle in the virtual 3D space based at least in part on the relative orientation of the first medical device with respect to the expected location of the user.

15. The system of claim 9, wherein the computing device is further configured to:

receive an indication of a point of interest;

mark, in an underlying 3D model, an intersection of a trajectory of the first medical device and a 2D plane corresponding to the 2D image area as the point of interest; and

cause the one or more displays to display in real-time a perspective view of the point of interest in the virtual 3D space based at least in part on the determined perspective view of the 2D image area.

16. The system of claim 9, wherein the first medical device comprises a needle and the second medical device comprises an imaging device.

17. A non-transitory computer-readable medium comprising computer-executable instructions, said instructions, when executed, cause one or more processors to:

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determine real-time position and orientation of a first medical device based at least in part on data received from a first pose sensor;

determine real-time position and orientation of a second medical device based at least in part on data received from a second pose sensor;

determine position and orientation of a 2D image area based at least in part on the determined real-time position and orientation of the second medical device;

receive image data for the 2D image area from the second medical device;

determine a perspective view of the 2D image area in a virtual 3D space based at least in part on a relative orientation of the second medical device with respect to an expected location of a user, wherein the expected location of the user is a fixed location in front of one or more displays; and

cause the one or more displays to display in real-time a perspective view of an image corresponding to the image data in the virtual 3D space based at least in part on the determined perspective view of the 2D image area.

18. The non-transitory computer-readable medium of claim 17, wherein said instructions, when executed, further cause one or more processors to:

receive an indication of a point of interest;

mark in an underlying 3D model an intersection of a trajectory of the first medical device and a 2D plane corresponding to the 2D image area as the point of interest; and

cause the one or more displays to display in real-time a perspective view of the point of interest in the virtual 3D space based at least in part on the determined perspective view of the 2D image area.

19. The non-transitory computer-readable medium of claim 17, wherein said instructions, when executed, further cause one or more processors to cause the one or more displays to display a 2D view of the image corresponding to the image data.

20. The non-transitory computer-readable medium of claim 17, wherein said instructions, when executed, further cause one or more processors to cause the one or more displays to display a graphic indicating an intersection between a trajectory of the first medical device and a location on a 2D plane corresponding to the 2D image area, wherein the location on the 2D plane is outside the 2D image area.

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